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**Title:** How does orientation-tuned normalization spread across the visual field?

**Running head:** Orientation-tuned normalization spread across visual field

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## Abstract

Visuocortical responses are regulated by gain control mechanisms, giving rise to fundamental neural and perceptual phenomena such as surround suppression. Suppression strength, determined by the composition and relative properties of stimuli, controls the strength of neural responses in early visual cortex, and in turn, the subjective salience of the visual stimulus. Notably, suppression strength is modulated by feature similarity; for instance, responses to a center-surround stimulus in which the components are collinear to each other are weaker than when they are orthogonal. However, this feature-tuned aspect of normalization, and how it may affect the gain of responses, has been understudied. Here, we examine the contribution of the tuned component of suppression to contrast response modulations across the visual field. To do so, we used functional magnetic resonance imaging (fMRI) to measure contrast response functions (CRFs) in early visual cortex (areas V1 – V3) in 10 observers while they viewed full-field center-surround gratings. The center stimulus varied in contrast between 2.67-96%, and was surrounded by a parallel or orthogonal surround at full contrast. We found substantially stronger suppression of responses when the surround was parallel to the center, manifesting as shifts in the population CRF. The magnitude of the CRF shift was strongly dependent on voxel spatial preference, and seen primarily in voxels whose receptive field spatial preference corresponds to the area straddling the center-surround boundary in our display, with little-to-no modulation elsewhere.

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### **New and Noteworthy**

Visuocortical responses are underpinned by gain control mechanisms. In surround suppression, it has been shown that suppression strength is affected by the orientation similarity between the center and surround stimuli. In this study, we examine the impact of orientation-tuned suppression on population contrast responses in early visual cortex and its spread across the visual field. Results show stronger suppression in parallel stimulus configurations, with suppression largely isolated to voxels near the center-surround boundary.

**Keywords:** vision, divisive normalization, surround suppression, contrast response functions, fMRI

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## Introduction

69           Visual perception is heavily influenced by context – a principle exemplified by the  
70 perceptual phenomenon known as surround suppression. Under surround suppression,  
71 the perceived contrast of a stimulus is attenuated in the presence of a surrounding  
72 stimulus (1–3). Surround suppression’s neural underpinnings are typically observed in  
73 animal electrophysiological recordings as decreases in central receptive field (RF)  
74 responses when an annulus is placed within its extraclassical surround (4–10).

75           While the addition of a surround stimulus is typically suppressive (5, 6, 8–10), the  
76 specific properties of the center and surround stimuli dictate the degree to which  
77 suppression will occur (11, 12). Specifically, suppression strength appears to be  
78 governed by the relative feature similarity between the two components, with the  
79 strongest suppression occurring when the surround and central stimuli are matched in  
80 orientation and spatial frequency (5, 10, 13–15). This feature-tuned component of  
81 suppression has been proposed to serve a number of functional roles in cortex, such as  
82 facilitating the use of spatial context to parse visual scenes – supporting redundancy  
83 reduction and efficient neural coding (11, 16).

84           Computationally, the influence of the surround on the center is well accounted for  
85 as a form of divisive modulation (5, 17, 18), in which the excitatory drive from the center  
86 stimulus is divided by a proportional suppressive drive, comprised of a more broadly  
87 spatially-tuned pool of units responding to both the center and the surrounding region  
88 of space. Divisive normalization (17, 19) has been put forth as a putative canonical  
89 computation, providing an explanatory account of a variety of nonlinear behaviors  
90 observed within visuocortical neurons, including surround suppression (17).

91 Another key feature of normalization models is their ability to describe the  
92 nonlinear relationship between a stimulus's contrast and its subsequent neural response  
93 (4, 17) – a relationship commonly referred to as the contrast response function (CRF) (20,  
94 21). While surround suppression has long been characterized as a signature of  
95 normalization, neuroimaging studies have been hindered by a lack of proper  
96 quantification of suppressive effects on the contrast response (22, 23), both within and  
97 across early visual areas. While previous neuroimaging work from our lab and others  
98 have consistently found suppression of responses when pairs of stimuli are aligned in a  
99 collinear configuration, compared to orthogonal (13, 14, 24–27), it is still unclear how  
100 surround suppression interacts with the population-level CRF.

101 In this study, we sought to identify changes in the gain underlying orientation-  
102 tuned suppression, both *within* and *across* early visual cortices. To do so, we presented  
103 participants with center-surround stimuli and measured changes in BOLD response as  
104 we parametrically varied the contrast of the center. Specifically, we varied the contrast  
105 of a central grating stimulus at 9 contrast levels, while the center was surrounded by a  
106 large, full contrast annulus grating that was either collinear or orthogonal in its orientation  
107 content relative to the center stimulus. We found that the contrast response functions of  
108 voxels with population receptive fields far from the center-surround boundary were not  
109 influenced by the orientation of the surround. However, the contrast response of voxels  
110 that were spatially selective to the center-surround boundary exhibited a gain shift to the  
111 collinear surround, relative to orthogonal. These results suggest that the effects of tuned  
112 normalization on the gain of responses within human visual cortex are spatially local to  
113 the areas of competition, rather than across the entire center stimulus representation.

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## Methods

### 115 Observers

116 Ten observers (8 female) took part in the experiment. All were between the ages  
117 of 18-35 and reported normal or corrected-to-normal visual acuity. All participants gave  
118 their written informed consent, and the study was approved by the Boston University  
119 Institutional Review Board. Observers received monetary compensation for their  
120 participation, except one (one of the authors of the study).

### 121 Apparatus and Stimuli

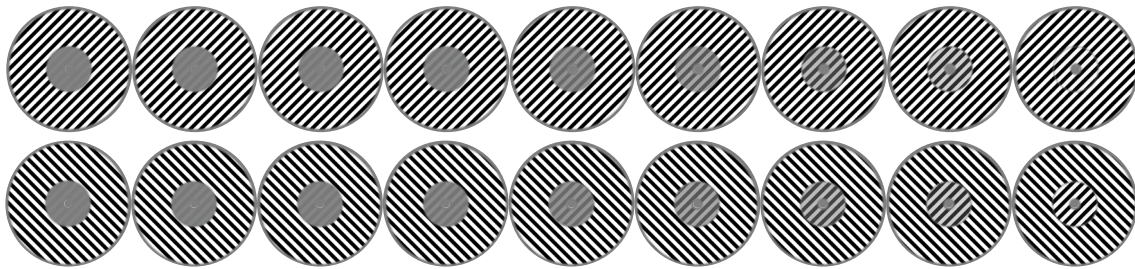
122 Stimuli were programmed and rendered on a MacBook Pro (OS X 10.7) using  
123 MATLAB (2015b; Mathworks, Natick, MA) and Psychophysics Toolbox (Brainard, 1997).  
124 The stimuli were displayed on a rear-projection screen in the scanner bore, using a  
125 gamma-corrected projector (ProPixx DLP LED, VPixx Technologies; max. luminance 306  
126  $\text{cd/m}^2$ ) and observers viewed them via a front-surface mirror affixed to the head coil.  
127 Participants were provided with a 2-button box for behavioral responses.

128 The visual stimulus was a 2 cycles/degree (cpd) center grating (inner radius 0.75  
129 dva from central fixation, outer radius 2.95 dva), which varied in contrast throughout  
130 each fMRI run, surrounded by a 2 cpd annular grating (inner radius 3.05 dva, outer radius  
131 8.5 dva), with a 0.1 dva gap between the central and surround component (**Figure 1A**).  
132 The small gap was chosen based on prior work which found strongest center-surround  
133 interactions with minimal spatial separation between the two components (1, 28–30).  
134 Prior work also informed the eccentric location of the center-surround boundary;  
135 surround suppression tends to be stronger when stimuli are presented away from fovea  
136 (2). Both gratings were embedded in a Gaussian envelope. The contrast of the center

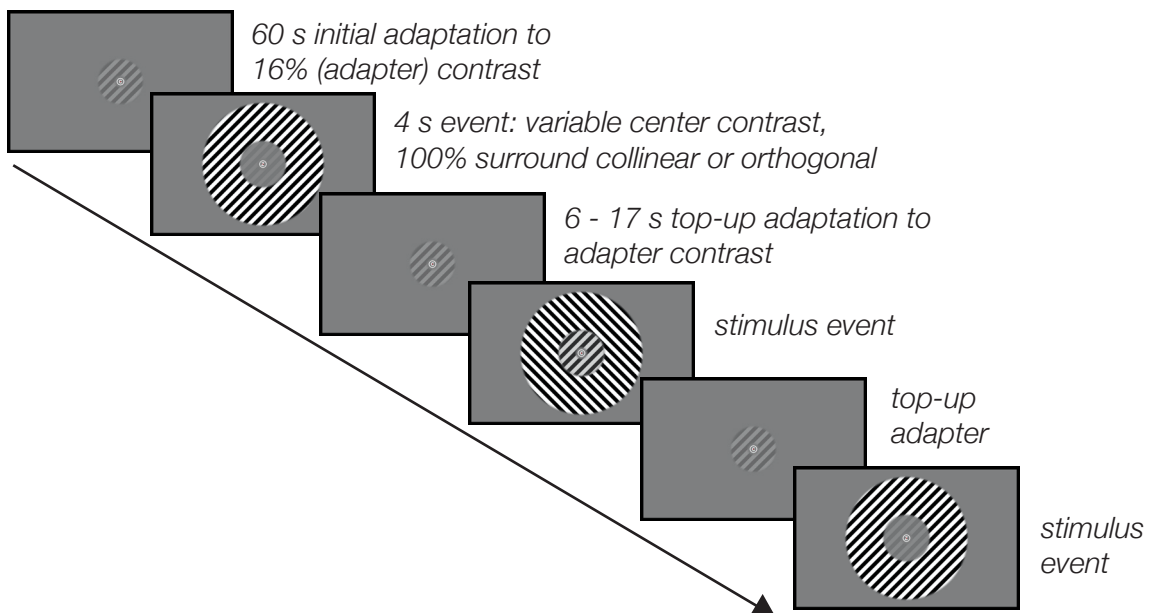
137 grating varied over nine logarithmically spaced contrast levels (2.67%, 4.0%, 5.33%,  
138 8.0%, 16%, 32%, 48%, 64%, 96% Michelson contrast), while the surround grating  
139 contrast was always 100% Michelson contrast. Both gratings had their spatial phase  
140 updated every 100 ms to a randomly chosen value, independently of each other. The  
141 surround grating could either be collinear or orthogonal with respect to the center. The  
142 central grating orientation remained identical throughout each run, and was either 45° or  
143 135° in alternating runs, with starting orientation counterbalanced between observers.  
144 Stimuli were presented on a mean luminance background.

145

**A**



**B**



146 *Figure 1.* (A) Experimental stimuli. Center contrast increases from left to right. Upper row: collinear  
147 surround, lower row: orthogonal surround. (B) Three example trials occurring at the start of a scan.  
148 Following the 60 s adaptation period, trial order is pseudo-randomized, and inter-trial intervals serve  
149 as top-up adapters to the 16% adapter contrast. In this example, the center grating orientation is  
150 45°. Note that spatial frequency was lowered for illustration purposes.

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## 152 **MRI data acquisition**

153 All MRI data were collected at the Center for Cognitive Neuroimaging center at  
154 Boston University on a Siemens 3T Prisma scanner with a 64-channel head coil. In a  
155 single two-hour session. fMRI data were acquired with simultaneous multi-slice (multi-  
156 band acceleration factor 5) echoplanar T2\*-weighted sequence (voxel size 2mm<sup>3</sup>, TR =  
157 1,000 ms, TE = 30 ms, flip angle = 64°, FOV = 208 × 208 × 140 mm). Prior to this session,  
158 each participant also went through a separate population receptive field (pRF) mapping  
159 session using the same T2\*-weighted protocol, in addition to a high-resolution  
160 anatomical scan (T1-weighted multi-echo MPRAGE sequence, FOV = 256 × 256 × 176  
161 mm, 36 slices, TR = 2530 ms, TE = 1.69 ms, FA = 7°, voxel size = 1mm<sup>3</sup>).

## 162 **Experimental procedure**

163 **Main task.** The main task had 498 TRs (1 s TR), and most participants completed 10  
164 runs (one completed 8, and two completed 9). Stimuli were presented in an event-related  
165 design, with 4 s event duration and jittered inter-trial interval between 6-17 s. The event  
166 schedules were generated using the FreeSurfer tool Optseq2 (31). To promote nonlinear  
167 contrast response functions, we used a contrast adaptation paradigm previously  
168 established in our lab (23, 32). Following a 4 s baseline period with a mean luminance  
169 screen, the phase-jittered central grating was presented for 60 s at 16% contrast  
170 (adapting contrast) in an initial adaptation block. Following this initial adaptation, the



171 event-related stimulus presentation began. During the stimulus event, the center grating  
172 changed contrast to the target contrast for that event, and was surrounded by either a  
173 collinear or orthogonal 100% contrast grating. The inter-trial intervals served as top-up  
174 adaptation periods, during which the center grating again changed contrast to the  
175 adapting contrast intensity. An example stimulus sequence is depicted in **Figure 1B**.  
176 Each of the 9 center contrast levels (including the adapting contrast) was presented four  
177 times within an fMRI run, twice with a collinear surround and twice with an orthogonal  
178 surround.

179 Participants were engaged in a rapid letter detection and identification task at  
180 fixation. The small (0.1 dva) fixation dot in the center of the screen was red, and  
181 surrounded by a white circular 1.5 dva diameter annulus. White letters were displayed  
182 within this annulus, in front of the fixation point, continuously throughout the run.  
183 Participants' task was to monitor this letter stream for letters 'J' and 'K' amid 10 other  
184 distractor letters ('X', 'L', 'V', 'H', 'S', 'A', 'C', 'P', 'Z', 'Y'). A new letter was presented  
185 every 200 ms, and participants were asked to press the left button on the response box  
186 as soon as they detected 'J', and the right button for 'K'. At the end of each run,  
187 performance accuracy was displayed to the participants for feedback. Accuracy across  
188 participants was 90.2% on average ( $\pm 2.4\%$  SEM).

189 **Functional localizer.** Each session began with two runs of a functional localizer,  
190 intended to isolate voxels responding to the center and the surround stimulus areas of  
191 the visual field. The localizer had a stimulus on (16 s) – stimulus off (16 s) blocked design,  
192 with 208 TRs (1 s TR), with each scan beginning and ending with an off block. The  
193 localizer stimulus was a 100% Michelson contrast, achromatic checkerboard

194 (fundamental frequency: 2 cpd) with the same inner and outer diameter as the main  
195 stimulus, on a mean luminance background, and the behavioral task was identical to the  
196 main experiment. Following the localizer runs, participants began the main task.

197 **Population receptive field mapping session.** For each observer, pRF mapping was  
198 carried out in a separate session, using stimuli and analysis code from the analyzePRF  
199 toolbox (33). In a single session, each observer underwent 10 pRF mapping runs (300  
200 TRs, 1s TR), which alternated 5 sweeping bar stimulus runs and 5 runs with a  
201 combination of rotating wedge and expanding and contracting ring. The results of  
202 analyzePRF were used to manually draw cortical surface labels outlining early visual  
203 areas V1, V2, and V3, by identifying polar angle preference reversals. The early visual  
204 area labels then served as a tool in voxel selection for functional data analysis.

## 205 **MRI data analyses**

206 **Anatomical data.** The 1 mm<sup>3</sup> T1 images acquired during the pRF mapping session were  
207 analyzed in FreeSurfer using the recon-all pipeline. The results were used to register the  
208 functional data to the anatomical data.

209 **fMRI preprocessing and beta weight estimation.** Reverse-phase encoding (34) was  
210 used to correct EPI distortion in the functional data in FSL (35). Following distortion  
211 correction, data were preprocessed with FS-FAST (36) with no spatial smoothing (FWHM  
212 = 0 mm), implementing standard motion correction, Siemens slice timing correction, and  
213 boundary-based registration (37). We used robust rigid registration (38) to achieve  
214 accurate voxel-to-voxel correspondence between functional runs within a session,  
215 aligning the middle TR of each run to the middle TR of the first run of the session. To  
216 identify voxels responsive to the stimuli, the functional localizer data for each localizer

217 type (center and surround) were analyzed in FreeSurfer with a GLM analysis following  
218 robust registration. The main task data were further processed using custom MATLAB  
219 scripts. We extracted voxels that fell within the pRF labels V1, V2, and V3. Following the  
220 removal of the beginning 64 TRs from each run (the 4 s initial baseline + the 60 s initial  
221 adaptation period), the time series data were low-pass filtered (filter cutoff 0.01 Hz),  
222 converted to % signal change by dividing the BOLD signal at each time point by the  
223 average BOLD signal value of the run, and concatenated.

224 We constrained our voxel inclusion as follows: first, we selected only voxels  
225 responding to either the center or surround localizer, defined as a GLM p-value of 0.05  
226 or less. Out of these voxels, we further selected only those with a pRF variance explained  
227 ( $R^2$ ) of 0.1 or above, and those whose eccentricity estimates fell within the stimulus  
228 bounds (i.e., between 0.75 and 8.5 dva). Furthermore, we ensured that voxels whose  
229 region of interest label overlapped were removed to avoid the inclusion of duplicate  
230 voxels in the dataset. After the application of these criteria, we had on average  $719 \pm$   
231  $174$  (SD) voxels in V1,  $485 \pm 88$  in V2, and  $335 \pm 42$  in V3.

232 **Contrast response estimation.** After finalizing the initial voxel selection, we  
233 implemented a voxel-wise finite impulse response (FIR) analysis in MATLAB, with a  
234 window size of 20 s following stimulus onset, resulting in 20 beta weight estimates for  
235 each condition (center-surround orientation offset and center contrast level). Finally, we  
236 computed the mean beta weight in each condition within an averaging window of 4 – 8  
237 TRs after stimulus onset, accounting for the hemodynamic response delay and capturing  
238 the peak of the hemodynamic response function for each observer and condition,

239 resulting in a voxel-wise contrast response function of 9 points (contrast levels) per  
240 condition.

241 **Contrast response function model fitting.** The contrast response function was fit with  
242 a variant of the Naka-Rushton equation (20, 21):

$$243 \quad R(c) = R_{max} \frac{c^n}{c^n + C_{50}^n} + b$$

244 Here, the BOLD response ( $R$ ) at each contrast level ( $c$ ) is determined by the maximum  
245 attainable response ( $R_{max}$ ), the contrast at the semi-saturation point (the semi-saturation  
246 constant,  $C_{50}$ ), an exponent ( $n$ ), and an additive baseline parameter ( $b$ ). MATLAB's  
247 *fmincon* function was used to implement the fit. We constrained the  $R_{max}$  parameter to  
248 be between 0 and 10 (beta weight, or % signal change), and the  $C_{50}$  parameter to be  
249 between 1 and 80 (% contrast). The baseline parameter was fixed per voxel to the  
250 average of the voxel's responses to the lowest contrast between the collinear and the  
251 orthogonal surround condition. Furthermore, we did not anticipate significant changes  
252 in the  $n$  parameter based on existing literature (4–6, 10); therefore, we opted to fix the  
253 value of  $n$  to 2 in each voxel (17, 39). The fitting procedure converged on a solution for  
254 all voxels. A goodness-of-fit estimate was obtained by computing the  $R^2$  of the Naka-  
255 Rushton fit for each voxel. We excluded voxels where the Naka-Rushton  $R^2$  was negative  
256 in either condition ( $40.7 \pm 5.1\%$  SD in V1,  $49 \pm 6.8\%$  in V2, and  $47 \pm 10.9\%$  in V3). The  
257 outer four eccentricity bins contributed the majority of these low- $R^2$  voxels, reflecting flat  
258 contrast responses to the full-contrast surround annulus. Model fitting was conducted  
259 in MATLAB, while most statistical tests were performed in R.

260 **Eye position monitoring**

261 Throughout the experimental session, participants' gaze was monitored using an  
262 MR-compatible eye-tracking setup (EyeLink 1000, SR Research, Ontario, Canada) with  
263 a sampling rate of 1,000 Hz (3 observers) or 500 Hz (7 observers). After excluding blinks,  
264 the average eye deviation from the fixation point in the center of the screen across  
265 participants was  $0.21 \text{ dva} \pm 0.09 \text{ dva SE}$  in horizontally and  $0.2 \text{ dva} \pm 0.11 \text{ dva SE}$   
266 vertically. This is well within the bounds of the fixation circle, whose radius was 0.75 dva.  
267 Therefore, participants maintained reliable fixation throughout the experimental session.

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## Results

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### **Contrast response functions under orientation-tuned suppression**

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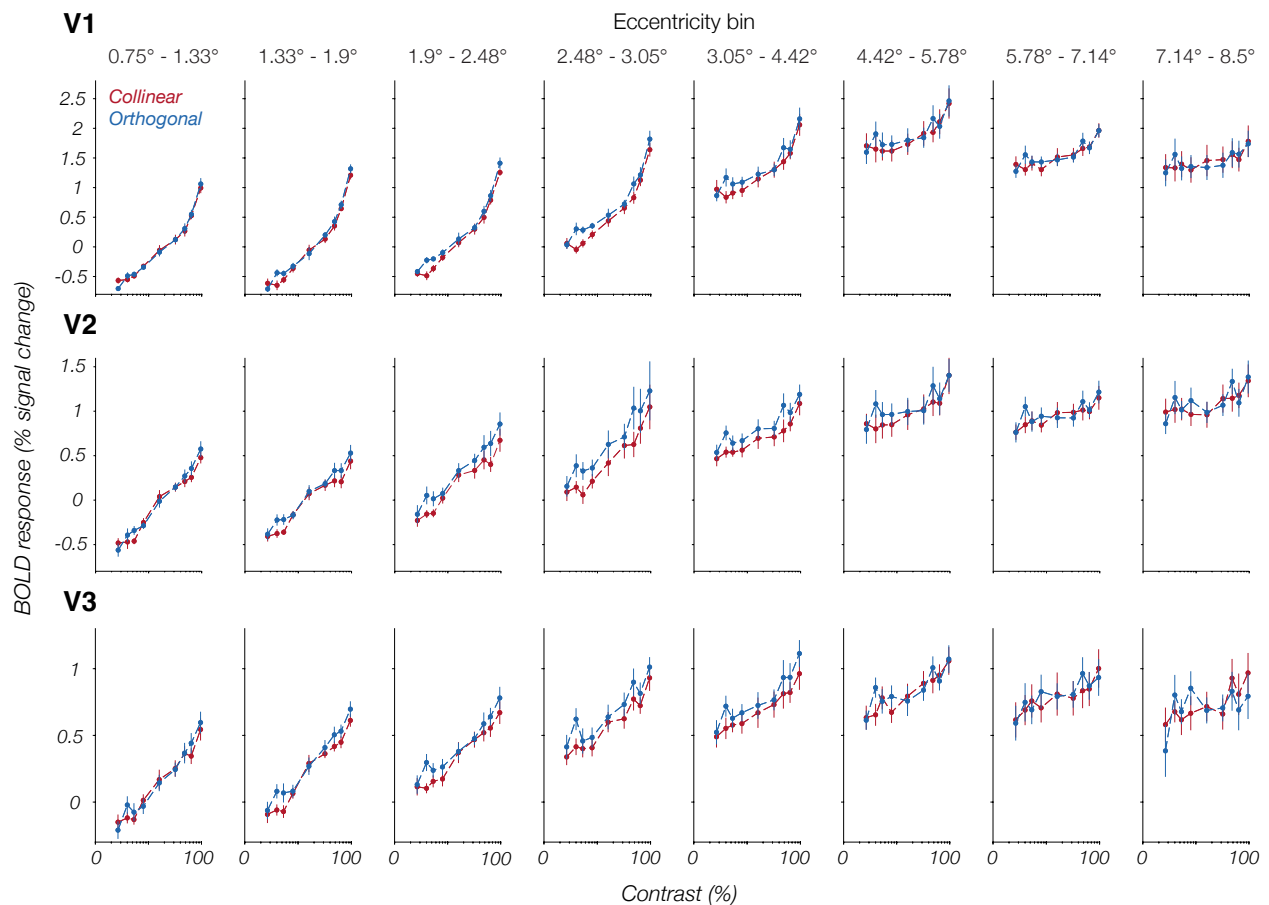
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Given the spatial layout of our full-field stimulus, we reasoned that any orientation-tuned modulation would be most apparent for voxels whose pRF location (eccentricity) is near the center-surround boundary. Instead of averaging the voxel-wise CRFs across the whole ROI, we binned the voxels into 8 bins based on their pRF preferred eccentricity. We first divided the stimulus into two portions: center (between 0.75 and 3.05 dva radius) and surround (between 3.05 and 8.50 dva radius), with the inner radius of the surround stimulus serving as the dividing line. We then divided each half of the display into four equal-sized eccentricity bins. As depicted in **Figure 2**, there was gradual gain modulation in the central portion of the stimulus; in the bin closest to fixation, the contrast responses to the collinear and orthogonal flanked condition largely overlap. The responses begin to diverge as a function of distance to the center-surround boundary, with largest gain modulation in the fourth bin (the center stimulus band abutting the surround). Differences between collinear and orthogonal condition persist in the first

284 surround bin, but the outermost bins show flatter responses for both conditions (due to  
285 the contrast of the surround remaining unchanged), which again largely overlap.

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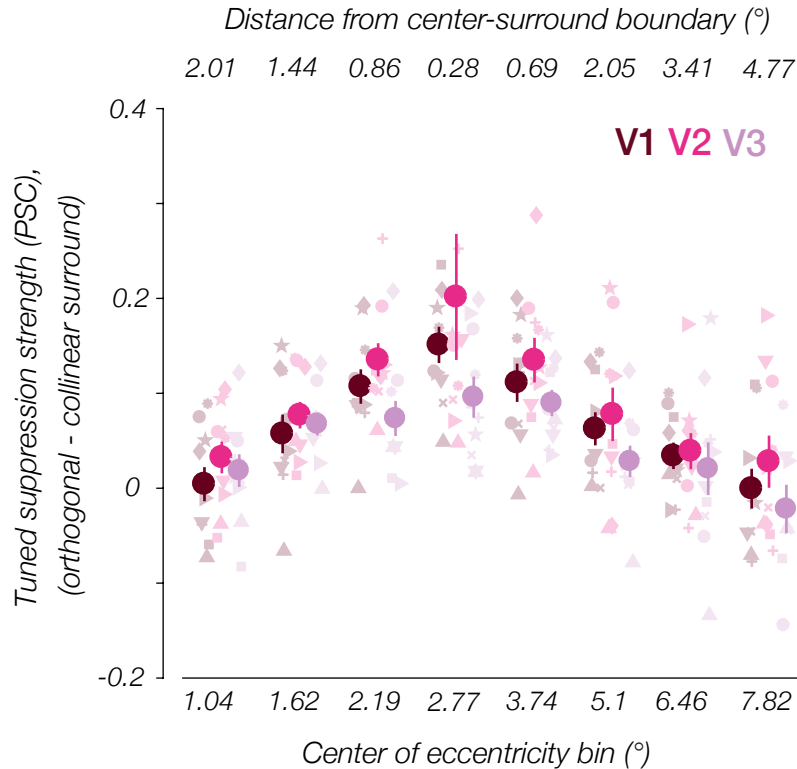


291 *Figure 2. Averaged eccentricity-binned contrast responses. Each row summarizes results from one*  
292 *visual area; V1: upper row, V2: middle row, V3: bottom row. Left four columns represent the four*  
293 *eccentricity bins into which the center stimulus was divided, right four columns show the four bins of*  
294 *the surround annulus. The bounds of each eccentricity bin are listed above the columns. Center-*  
295 *surround boundary is located at 3.05° from fixation. The plots were obtained by averaging the %*  
296 *signal change across all voxels per observer (N = 10) in each bin, and then computing between-*  
297 *observer averages in each condition for that bin (red: collinear, blue: orthogonal). Error bars represent*  
298 *± 1 SEM.*

299

### 300 **Orientation-tuned suppression across the visual field**

301 To quantify the relationship between gain modulation and voxel position relative  
302 to the center-surround boundary, we computed the average overall tuned suppression  
303 strength in each eccentricity bin. First, we averaged the voxel-wise % signal change  
304 across contrast levels. Overall suppression was computed by subtracting the % signal  
305 change in the collinear surround from the orthogonal surround. Observer-averaged gain  
306 modulation as a function of voxel placement within the stimulus is depicted in **Figure 3**.  
307 Gain modulation in the center stimulus (first four bins) gradually increases across  
308 eccentricity and reaches maximum in the center stimulus band neighboring the  
309 surround. A mixed linear model (observers as random effects) including all voxels in our  
310 sample revealed that the absolute distance from the center-surround boundary at  $3.05^\circ$   
311 (in dva) significantly predicted orientation-tuned suppression strength (beta = -0.042,  
312 95% CI [-0.04, -0.04],  $t(84844) = -9.90$ ,  $p < 0.001$ ), confirming that the differences in %  
313 signal change were largest near the center-surround boundary. The effects of ROI were  
314 also significant; compared to V1, tuned normalization effects were more pronounced in  
315 V2 (beta = 0.02, 95% CI [0.02 0.02],  $t(84844) = 13.02$ ,  $p < 0.001$ ), and less pronounced  
316 in V3 (beta = -0.01, 95% CI [-0.02 -0.01],  $t(84844) = 9.90$ ,  $p < 0.001$ ).



317 *Figure 3.* Tuned suppression as a function of voxel position within the center-surround stimulus. First,  
 318 the voxel-wise average BOLD response across all contrast levels was computed in each stimulus  
 319 eccentricity bin in both conditions (collinear vs. orthogonal surround). We subsequently subtracted  
 320 the averaged BOLD response in the collinear surround condition from the orthogonal surround BOLD  
 321 response for each participant, and averaged across participants (N = 10) in each bin. The leftmost  
 322 data points represent the eccentricity bin closest to fixation. The center-surround boundary (3.05°) is  
 323 between the fourth (outermost center) and fifth bin (innermost surround). Error bars represent  $\pm 1$   
 324 SEM. (PSC = % signal change).

325

### 326 **Quantifying contrast response function modulations**

327 The variability of voxel-wise CRFs, and hence, that of Naka-Rushton parameters,  
 328 was substantial in all three visual areas. While most voxels had non-linear CRFs, many  
 329 CRFs did not saturate at high contrasts, likely due to stimulus optimality issues (see  
 330 Discussion). Out of the total of 2,026 voxels fulfilling our center-surround boundary  
 331 criteria, 865 did not show saturation in at least one condition; we defined this as a  $C_{50}$   
 332 value above 75% contrast, to reflect the fact that most of these voxels'  $C_{50}$  estimate was



333 very close to the fitting algorithm upper constraint of 80%, suggesting that the true best-  
334 fitting  $C_{50}$  would have been outside of the range of possible contrasts were the fitting not  
335 constrained by an upper boundary. With this caveat, we conducted exploratory analyses  
336 to more closely investigate the nature of CRF gain modulation across voxels.

337 In order to compare the voxel-wise Naka-Rushton parameters between the two  
338 surround configurations, we selected voxels based on whether the extent of their pRFs  
339 included the boundary between the center and the surround. For each voxel, we added  
340 and subtracted the pRF size estimate to/from the voxel's pRF eccentricity estimate, to  
341 obtain approximate coverage of the pRF within the stimulus. Across participants, on  
342 average 109 ( $\pm$  48 SD) voxels in V1, 51 ( $\pm$  14) voxels in V2, and 43 ( $\pm$  10) voxels in V3  
343 fulfilled this criterion. The average eccentricity of the center of the voxels' pRF was 3.18°  
344 from fixation across ROIs ( $\pm$  0.71° SD). In this subset, we compared collinear vs.  
345 orthogonal median  $C_{50}$  and  $R_{max}$  estimates in each ROI using a one-sided pairwise  
346 Wilcoxon test (reflecting our reasoning that if suppression is stronger in the collinear  
347 configuration, we should see a higher  $C_{50}$  in this condition, and/or a lower  $R_{max}$ , as seen  
348 in electrophysiology).  $C_{50}$  was overall higher in the collinear condition; however, this  
349 difference reached significance only in V2 ( $Z = -2.25$ ,  $p = 0.012$ , after Bonferroni  
350 correction to the number of ROIs).  $R_{max}$  did not differ between conditions in any ROI.

351 We additionally modeled  $C_{50}$  and  $R_{max}$  (in separate models) as predicted by  
352 surround orientation and ROI in mixed-effects models. In predicting the values of the  
353 semi-saturation parameter, the effect of surround orientation was statistically significant,  
354 confirming lower  $C_{50}$  in the orthogonal condition (beta = -8.34, 95% CI [-10.12, -6.57],  
355  $t(4046) = -9.19$ ,  $p < 0.001$ ). Similarly, the effect of ROI was significant, with overall lower

356  $C_{50}$  in V2 (beta = -14.82, 95% CI [-17.02, -12.61],  $t(4046) = -13.18$ ,  $p < 0.001$ ) and V3  
357 (beta = -10.82, 95% CI [-13.15, -8.48],  $t(4046) = -9.07$ ,  $p < 0.001$ ) compared to V1. For  
358  $R_{max}$ , the effect of surround orientation was not statistically significant, while a significant  
359 effect of ROI reflected lower  $R_{max}$  in V2 (beta = -0.81, 95% CI [-0.91, -0.70],  $t(4046) = -$   
360 14.57,  $p < 0.001$ ) and V3 (beta = -1.12, 95% CI [-1.24, -1.01],  $t(4046) = -19.14$ ,  $p < 0.001$ )  
361 compared to V1. However, the model fits, and therefore, explanatory power, were only  
362 weak to moderate ( $R^2$  for the  $C_{50}$  model was 0.13 and for the  $R_{max}$  model, 0.14).

363

364

## Discussion

365 We investigated how orientation-tuned suppression modulates the gain of  
366 visuocortical contrast responses, by measuring early visual BOLD signal modulations to  
367 a contrast-varying center grating surrounded by a full contrast annulus either collinear  
368 or orthogonal to the center. We found gain modulation in the collinear surround  
369 configuration compared to orthogonal, with lower BOLD responses and population CRF  
370 shifts relative to orthogonal. Extrastriate cortex generally showed stronger gain  
371 modulation by parallel surround relative to orthogonal, compared to V1. Orientation-  
372 dependent CRF shifts were observed predominantly in voxels whose pRF location and  
373 size positioned them such that they received stimulation from both center and surround  
374 stimuli, and was maximal in center voxels directly bordering the surround annulus. Near-  
375 foveal voxels instead showed strong overlap between the collinear and orthogonal CRFs.  
376 This pattern suggests that gain modulation by orientation-tuned suppression from the  
377 surround is spatially local, as opposed to spreading to the entire center stimulus.

378 Broadly, our findings are in agreement with prior fMRI studies in early visual areas  
379 demonstrating the orientation dependency of surround suppression, in which parallel  
380 surrounds induced stronger BOLD signal suppression compared to orthogonal  
381 surrounds (13, 14, 25, 27, 40). Past fMRI results complement psychophysical studies of  
382 surround suppression, in which the apparent contrast of a central stimulus is lower in  
383 the presence of a high-contrast surround (1–3, 41), and this suppressive effect is  
384 stronger with collinear surrounds as compared to orthogonal (1, 2, 41). When it comes  
385 to breaking down the surround suppression effects across the visual field, to our  
386 knowledge, there is limited work directly examining how magnitude of perceptual  
387 suppression might vary across the center in a center-surround stimulus, and instead it  
388 is largely assumed the perceived contrast of the center stimulus (and the underlying  
389 neural response) is constant across its area. One psychophysical study (42) found that  
390 when the innermost portion of a central grating in a center-surround stimulus is removed,  
391 thus forcing participants to use the edge of the center abutting the surround for contrast  
392 detection, thresholds increased similarly to a regular center-surround configuration,  
393 suggesting that the effect of a high-contrast surround stimulus extends slightly beyond  
394 its area. Our participants did not indicate any differences in perceptual suppression  
395 strength between the innermost areas of the center stimulus and those closer to the  
396 surround annulus. Future work could address whether there are psychophysical  
397 differences in suppression strength as a function of distance from the suppressing  
398 stimulus, or whether there is a perceptual filling-in effect at play which is not reflected in  
399 the early visual BOLD responses.

400           Mirroring prior electrophysiological work, we see considerable variability among  
401 individual CRF measurements (4–6, 8–10, 43). In electrophysiology, neuronal CRFs are  
402 fit with the Naka-Rushton equation, a variant of the normalization model. The two most  
403 commonly observed CRF modulations as a result of placement of a suppressive  
404 surround are contrast gain (a rightward shift of the CRF and a corresponding increase in  
405 the semi-saturation constant), and response gain (compression of the CRF at high  
406 contrasts, and a decrease in the maximum response). Contrast gain is thought to bring  
407 the most sensitive portion of the CRF towards the ambient contrast level (44), thereby  
408 optimizing the sensitivity of the neuron through divisive computations, while response  
409 gain decreases responsiveness at higher contrasts. Prior studies mostly report a mixture  
410 of effects (5, 8), and more recent evidence has suggested that the type of modulation  
411 may be determined by the spatial frequency preference of the cell (45). In the current  
412 dataset, lack of CRF saturation in many voxels limits our ability to conclusively comment  
413 on the exact nature of voxel-wise gain modulation, although exploratory analyses  
414 indicate an increase in the semi-saturation constant in the collinear condition relative to  
415 orthogonal.

416           The lower rate of saturation in our data diverges somewhat from other fMRI  
417 studies utilizing adaptation to recover saturating nonlinearities in the population CRF (23,  
418 32). We suspect non-saturation in our data was caused by the relative lack of stimulus  
419 optimality for early visual cortex; specifically, we did not account for cortical  
420 magnification in the stimulus spatial frequency, which was done by Vinke et al. (2022),  
421 and the center grating stimulus was not oriented radially from fixation, as done in Vinke  
422 et al. (2022), and to some extent in Foster and Ling (2022). Our stimulus was instead

423 intended to maximize perceptual suppression from the high-contrast surround  
424 presentation.

425         A suggested purpose of feature-dependent surround suppression is to serve  
426 texture segmentation (11, 16, 46–48), and both differences in contrast and orientation  
427 signal the presence of areas of higher interest in a visual scene possibly containing  
428 borders between objects or textures. Suppressing signals from similar regions and  
429 enhancing signals from bordering regions with different textures is thought to achieve  
430 higher efficiency in transmitting information via visuocortical spikes (47, 48). Our results  
431 suggest this modulation is spatially local at the level of the early visual cortex, which  
432 comes as something of a surprise given that the perceptual effect of such center-  
433 surround configurations is that of a wholesale attenuation in perceived contrast.

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445 **Data availability:** Source data for this study are available at  
446 [https://osf.io/6z5j2/?view\\_only=ac2090feb71c488a8800d9e11ff4cce1](https://osf.io/6z5j2/?view_only=ac2090feb71c488a8800d9e11ff4cce1)

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454

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## Figure legends

627 Figure 1. (A) Experimental stimuli. Center contrast increases from left to right. Upper row:  
628 collinear surround, lower row: orthogonal surround. (B) Three example trials occurring at  
629 the start of a scan. Following the 60 s adaptation period, trial order is pseudo-  
630 randomized, and inter-trial intervals serve as top-up adapters to the 16% adapter  
631 contrast. In this example, the center grating orientation is  $45^\circ$ . Note that spatial frequency  
632 was lowered for illustration purposes.

633

634 Figure 2. Averaged eccentricity-binned contrast responses. Each row summarizes  
635 results from one visual area; V1: upper row, V2: middle row, V3: bottom row. Left four  
636 columns represent the four eccentricity bins into which the center stimulus was divided,  
637 right four columns show the four bins of the surround annulus. The bounds of each  
638 eccentricity bin are listed above the columns. Center-surround boundary is located at  
639  $3.05^\circ$  from fixation. The plots were obtained by averaging the % signal change across  
640 all voxels per observer ( $N = 10$ ) in each bin, and then computing between-observer  
641 averages in each condition for that bin (red: collinear, blue: orthogonal). Error bars  
642 represent  $\pm 1$  SEM.

643

644 Figure 3. Tuned suppression as a function of voxel position within the center-surround  
645 stimulus. First, the voxel-wise average BOLD response across all contrast levels was  
646 computed in each stimulus eccentricity bin in both conditions (collinear vs. orthogonal  
647 surround). We subsequently subtracted the averaged BOLD response in the collinear  
648 surround condition from the orthogonal surround BOLD response for each participant,

649 and averaged across participants ( $N = 10$ ) in each bin. The leftmost data points represent  
650 the eccentricity bin closest to fixation. The center-surround boundary ( $3.05^\circ$ ) is between  
651 the fourth (outermost center) and fifth bin (innermost surround). Error bars represent  $\pm 1$   
652 SEM. (PSC = % signal change).