

# Pupil-linked arousal modulates precision of stimulus representation in cortex

Abbreviated title: Arousal modulates sensory precision

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Conflict of interest statement

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## 1 ABSTRACT

2 Neural responses are naturally variable from one moment to the next, even when the stimulus is held  
3 constant. What factors might underlie this variability in neural population activity? We hypothesized  
4 that spontaneous fluctuations in the cortical stimulus representation are created by changes in arousal  
5 state. We tested the hypothesis using a combination of fMRI, probabilistic decoding methods and  
6 pupillometry. Human participants (20 female, 12 male) were presented with gratings of random  
7 orientation. Shortly after viewing the grating, participants reported its orientation and gave their level  
8 of confidence in this judgment. Using a probabilistic fMRI decoding technique, we quantified the  
9 precision of the stimulus representation in the visual cortex on a trial-by-trial basis. Pupil size was  
10 recorded and analyzed to index the observer's arousal state. We found that the precision of the cortical  
11 stimulus representation, reported confidence, and variability in the behavioral orientation judgments  
12 varied from trial to trial. Interestingly, these trial-by-trial changes in cortical and behavioral precision  
13 and confidence were linked to pupil size and its temporal rate of change. Specifically, when the cortical  
14 stimulus representation was more precise, the pupil dilated more strongly prior to stimulus onset and  
15 remained larger during stimulus presentation. Similarly, stronger pupil dilation during stimulus  
16 presentation was associated with higher levels of subjective confidence, a secondary measure of  
17 sensory precision, as well as improved behavioral performance. Taken together, our findings support  
18 the hypothesis that spontaneous fluctuations in arousal state modulate the fidelity of the stimulus  
19 representation in the human visual cortex, with clear consequences for behavior.

## 20 SIGNIFICANCE STATEMENT

21 The fidelity of our sensory experiences varies from moment to moment. For example, we sometimes  
22 fail to recognize a friend in a crowd or mistake them for someone else. What determines the quality  
23 of human sensation and perception? In this study, we investigated whether fluctuations in alertness  
24 might play a role. We recorded brain activity while participants viewed images and reported both what  
25 they had seen and how confident they felt in this judgment. We discovered that a spontaneous change  
26 in alertness impacts the fidelity of information processing in the visual brain as well as reported levels  
27 of confidence and behavioral performance. These findings provide new insight into the mechanisms  
28 that underlie spontaneous changes in sensory information processing in the human brain.

## 29 INTRODUCTION

30 Neural and behavioral responses are rarely constant over time – not even for repeated presentations  
31 of the same stimulus (see e.g. Faisal et al., 2008 for a review). While numerous processes underlie  
32 these apparent fluctuations in brain and behavior, spontaneous changes in arousal state likely play an  
33 outsized role in this variability. Arousal refers to a state of physiological alertness or readiness,  
34 mediated by brainstem neuromodulatory systems, with wide-spread influences on neural and  
35 physiological activity. Previous work has shown that arousal modulates overall activity in the visual  
36 cortex (Livingstone and Hubel, 1981; Reimer et al., 2014; Vinck et al., 2015; Roth et al., 2020) and even  
37 the retina (Schröder et al., 2020), but whether it influences the quality of sensory information  
38 processing remains unknown. Here, we propose that spontaneous fluctuations in arousal modulate  
39 the fidelity of stimulus representations in cortex. More specifically, we hypothesize that arousal  
40 enhances the precision with which sensory information is represented in neural population activity in  
41 the visual cortex.

42 To test this hypothesis, we measured cortical activity with functional magnetic resonance imaging  
43 (fMRI) while participants performed a perceptual judgment task, and recorded pupil size as an index  
44 of arousal. Pupil size is commonly used as an indicator of arousal state, motivated by the tight links  
45 between pupil dilator muscles and the locus coeruleus-norepinephrine (LC-NE) system (see Mathôt,  
46 2018, for a review), which is believed to play a central role in arousal (Moruzzi and Magoun, 1949;  
47 Aston-Jones and Cohen, 2005; Sara, 2009). Indeed, the relationship between pupil size and arousal has  
48 been demonstrated in both neurophysiological (Aston-Jones and Cohen, 2005; Varazzani et al., 2015;  
49 Joshi et al., 2016) and neuroimaging studies (Murphy et al., 2014). Activity in the LC-NE system is not  
50 only linked to pupil size per se, but is particularly tightly coupled with rapid (phasic) changes in pupil  
51 size (Reimer et al., 2016). In recent years, researchers have therefore started using the rate of change  
52 in pupil size, quantified as the first derivative or slope of the pupil signal, as an (additional) measure of

53 arousal (e.g. de Gee et al., 2020; Podvalny et al., 2021; Pfeffer et al., 2022). In this study, we consider  
54 both pupil size and its rate of change (slope).

55 To quantify the quality of the stimulus representation in the visual cortex, we applied a probabilistic  
56 decoding technique (van Bergen et al., 2015; van Bergen and Jehee, 2018). This method decodes  
57 stimulus information from a pattern of cortical activity as a probability distribution over all possible  
58 stimuli – on a per-trial basis. Importantly, the width of the decoded distribution provides a metric of  
59 the uncertainty associated with the cortical stimulus representation: the wider the decoded  
60 distribution, the wider the range of stimuli that are consistent with the activity pattern. Vice versa, a  
61 narrow decoded distribution suggests that only a few stimuli are likely to have triggered the given  
62 response pattern; in other words, the cortical representation of the stimulus is very precise. Previous  
63 work has shown that decoded uncertainty provides a reliable measure of the quality of the cortical  
64 representation of sensory information (van Bergen et al., 2015; van Bergen and Jehee, 2019; Li et al.,  
65 2021; Geurts et al., 2022; Chetverikov and Jehee, 2023). Because sensory uncertainty has been linked  
66 to the participant’s self-reported levels of confidence about their perceptual decisions (Geurts et al.,  
67 2022), we considered reported confidence as a secondary measure of sensory uncertainty. To assess  
68 arousal’s impact on behavior, we also quantified the precision of the participant’s behavioral responses  
69 across trials.

70 Using these methods, we found evidence to suggest that spontaneous fluctuations in pupil-linked  
71 arousal state modulate the fidelity of stimulus representations in the human visual cortex. Specifically,  
72 we observed that decoded uncertainty, reported levels of confidence and behavioral precision vary  
73 from moment to moment and are linked to both pupil size and its rate of change. These results support  
74 the hypothesis that arousal plays a role in modulating the quality of sensory representations in the  
75 human visual cortex.

## 76 MATERIALS AND METHODS

### 77 Participants

78 Thirty-two healthy adult volunteers (20 female, 12 male, age: 19-31 years) with normal or corrected-  
79 to-normal vision participated in this study, which was approved by the local medical ethics review  
80 committee (CMO Arnhem-Nijmegen, the Netherlands). All participants provided informed written  
81 consent and received monetary compensation for their participation. The sample size ( $N = 32$ ) was  
82 based on a power calculation for detecting a reliable correlation between decoded uncertainty and  
83 behavioral variability using data from a previous study with a similar design (van Bergen et al., 2015;  
84 power = 0.8;  $\alpha = 0.05$ ). Participants were included based on their ability to perform the task, which was  
85 assessed in a separate behavioral training session prior to the experimental sessions.

### 86 Imaging data acquisition

87 The MRI data were collected using a Siemens 3T MAGNETOM PrismaFit scanner and a 32-channel head  
88 coil at the Donders Centre for Cognitive Neuroimaging in Nijmegen, the Netherlands. The data were  
89 analyzed previously for a different purpose (Geurts et al., 2022). Each scan session started with the  
90 collection of T1-weighted image (3D MPRAGE; repetition time (TR): 2300 ms; inversion time (TI):  
91 1100 ms; echo time (TE): 3 ms; flip angle: 8 degrees; field of view (FOV), 256 mm  $\times$  256 mm;  
92 192 sagittal slices; 1-mm isotropic voxels) and B0 field inhomogeneity maps (TR: 653 ms; TE: 4.92 ms;  
93 flip angle: 60 degrees; FOV: 256 mm  $\times$  256 mm; 68 transversal slices; 2-mm isotropic voxels;  
94 interleaved slice acquisition). Functional MRI data were acquired using a multi-band accelerated  
95 gradient-echo EPI sequence, with 68 transversal slices covering the whole brain (TR: 1500 ms; TE:  
96 38.60 ms; flip angle: 75 degrees; FOV: 210 mm  $\times$  210 mm; 2-mm isotropic voxels; multiband  
97 acceleration factor: 4; interleaved slice acquisition).

## 98 Pupil data acquisition

99 Pupillometry data were acquired using an SR Research Eyelink 1000 system. Pupil size was sampled at  
100 1 kHz. Pupil recordings were collected for 62 out of 64 sessions, and only partially (4-12 runs out of a  
101 total of 10-13) for 11 of these sessions, due to technical difficulties.

## 102 Experimental design

103 Participants performed an orientation estimation task (Figure 1) inside the MRI scanner. They were  
104 instructed to maintain fixation on a black-and-white bullseye target (radius: 0.375 degrees) presented  
105 at the center of the screen throughout each run. Runs consisted of 20 trials each (trial duration: 16.5  
106 s, inter-trial interval: 1.5 s) and started and ended with a fixation period (duration: 4.5 and 16 s,  
107 respectively). Each trial began with the presentation of an orientation stimulus (duration: 1.5 s),  
108 followed by a 6-s retention interval, and two 4.5-s response windows in which observers were  
109 prompted to report the orientation of the viewed grating and indicate their level of confidence in this  
110 orientation response. The stimuli were counterphasing sinusoidal gratings (contrast: 10%; spatial  
111 frequency: one cycle per degree; randomized spatial phase; 2-Hz sinusoidal contrast modulation),  
112 presented inside an annulus around fixation (inner radius: 1.5 degrees; outer radius: 7.5 degrees;  
113 contrast linearly decreasing over the inner and outer 0.5 degrees of the annulus). Stimulus orientations  
114 were drawn pseudorandomly from a uniform distribution (0-179 degrees) to ensure an approximately  
115 even sampling of orientation within any given run. During the first response window, participants  
116 reported the orientation of the viewed grating by rotating a black bar (length: 2.8 degrees; width: 0.1  
117 degrees; contrast: 40%; initial orientation randomized across trials) presented at the center of the  
118 screen. During the second response window, participants indicated their confidence in this orientation  
119 judgment by sliding a white dot over a circular scale. The scale was a black bar of increasing width  
120 (contrast: 40%; bar width: 0.1–0.5 degrees, linearly increasing) that was wrapped around fixation  
121 (radius: 1.4 degrees). The mapping between confidence level and scale width (i.e., whether the narrow  
122 end of the scale indicated high or low confidence) was counterbalanced across participants, and the

123 orientation and direction of the scale (i.e., whether the width increased in clockwise or  
124 counterclockwise direction), as well as the dot's starting position, were randomized across trials. For  
125 both response windows, the response bar (or scale) faded linearly over the last 1 s of the response  
126 window to indicate the approaching end of this window, and participants responded using two buttons  
127 (one for clockwise and one for counterclockwise rotation) on an MRI-compatible button box. Each trial  
128 was preceded by the fixation bullseye briefly turning black (duration: 0.1 s, timing: -0.5 s relative to  
129 stimulus onset) as a cue to stimulus onset. Participants performed a total of 22-26 task runs inside the  
130 scanner, divided over two sessions on separate days, and extensively practiced the task in separate  
131 behavioral sessions prior to the experiment (2-4 hours in total).

132 Each scan session also included one or two functional localizer runs, in which flickering checkerboard  
133 stimuli (contrast: 100%, flicker frequency: 10 Hz, check size: 0.5 degrees) were presented within the  
134 same annulus as the orientation stimuli. Checkerboard stimuli were presented in seven 12-s blocks  
135 interleaved with fixation blocks of equal duration. In a separate scan session, retinotopic maps of the  
136 visual cortex were acquired using standard retinotopic mapping procedures (Sereno et al., 1995; Deyoe  
137 et al., 1996; Engel et al., 1997).

138 Visual stimuli were generated by a Macbook Pro computer using MATLAB and the Psychophysics  
139 Toolbox (Brainard, 1997; Kleiner et al., 2007), and displayed via a luminance-calibrated projector (EIKI  
140 LC-XL100; screen resolution: 1,024 × 768 pixels; refresh rate: 60 Hz) on a rear-projection screen, which  
141 the participants viewed via a mirror mounted on the head coil.

## 142 **Preprocessing of MRI data**

143 Preprocessing procedures for functional imaging data are also described in Geurts et al. (2022), and  
144 reproduced here for convenience. Motion correction was performed with respect to the middle  
145 volume of the middle run of each session (the motion correction template) with FSL's MCFLIRT  
146 (Jenkinson et al., 2002). The motion-correction template was corrected for distortions due to B0 field



147 inhomogeneities using the acquired field maps, and registered to a high-resolution anatomical (T1-  
148 weighted) image acquired in the same session using `epi_reg` within FSL's FLIRT (Jenkinson and Smith,  
149 2001). For co-registration of data across sessions, we created participant-specific anatomical  
150 templates by combining the anatomical reference images from the two separate sessions using  
151 Freesurfer's `mri_robust_template` (Reuter et al., 2012), to which the single-session anatomical images  
152 were registered. All transformations were then combined and applied to the raw data. To remove slow  
153 drifts in the MRI signal, the transformed data were temporally filtered using FSL's nonlinear high-pass  
154 filter (Jenkinson et al., 2012) with a sigma of 24 TRs (two trials), which corresponds to a cut-off of  
155 around 83 s. Residual motion effects were removed from the data through linear regression, using a  
156 set of 24 motion regressors derived from the motion parameters estimated by MCFLIRT.

157 The region of interest (ROI) for decoding (bilateral V1, V2, and V3, combined) was identified on the  
158 reconstructed cortical surface, obtained with Freesurfer's cortical reconstruction algorithm (Dale et  
159 al., 1999), using single-participant retinotopic maps (see *Experimental design*). For further analysis, we  
160 selected the 2000 voxels within this ROI that were most strongly activated by the functional localizer  
161 stimulus while surviving a lenient statistical threshold of  $p < 0.01$ , uncorrected. Voxel selection was  
162 performed for each participant individually in native space. Each voxel's timeseries were z-normalized  
163 with respect to corresponding trial time points in the same run. Finally, we obtained single-trial  
164 activation patterns by adding a 4.5-s temporal shift (to account for the hemodynamic delay) and then  
165 averaging over the first 3 s of each trial. Importantly, this time window excludes activity from the  
166 behavioral response window.

## 167 **Decoding algorithm**

168 To quantify the trial-by-trial precision of stimulus representations in visual cortex, we applied a  
169 generative-model based probabilistic decoding algorithm (van Bergen et al., 2015; van Bergen and  
170 Jehee, 2018) to our data (see *Preprocessing of MRI data* for voxel selection criteria). We provide a  
171 concise description of the decoding algorithm here, and refer the interested reader to previous

172 publications for further detail (van Bergen et al., 2015; van Bergen and Jehee, 2018). The decoding  
 173 model describes the across-trial distribution of activation patterns as a multivariate normal, centered  
 174 around a stimulus-specific mean that describes the tuning function of each voxel. Tuning functions  
 175 were modeled as a linear combination  $\mathbf{W}\mathbf{f}(s)$  of eight bell-shaped basis functions  $\mathbf{f}(s) =$   
 176  $[f_1(s), \dots, f_8(s)]^T$ , each centered on a different orientation (Brouwer and Heeger, 2009). The basis  
 177 functions are described as follows:

$$178 \quad f_k(s) = \max\left(0, \cos\left(2\pi \frac{s - \phi_k}{180}\right)\right)^5$$

179 in which  $s$  is the orientation of the presented stimulus and  $\phi_k$  is the center of the  $k$ th basis function.  
 180 Basis functions were spaced equally across the full orientation space (0-179 degrees) with the first one  
 181 centered at zero. The basis functions are weighted by coefficients  $\mathbf{W}$ , with  $W_{ik}$  the contribution of the  
 182  $k$ th basis function to the tuning function of the  $i$ th voxel.

183 The variance around the stimulus-dependent mean activation pattern (i.e., the multivariate tuning  
 184 function) is modeled by the covariance matrix:

$$185 \quad \mathbf{\Omega} = \rho \boldsymbol{\tau} \boldsymbol{\tau}^T + (1 - \rho) \text{diag}(\boldsymbol{\tau}^2) + \sigma^2 \mathbf{W} \mathbf{W}^T$$

186 The first component of the covariance matrix  $\rho \boldsymbol{\tau} \boldsymbol{\tau}^T$  models global fluctuations shared between all  
 187 voxels in the ROI. The second component  $(1 - \rho) \text{diag}(\boldsymbol{\tau}^2)$ , with  $\boldsymbol{\tau}^2 = [\tau_i^2]^T$ , describes independent,  
 188 voxel-specific variability (with variance  $\tau_i^2$  for voxel  $i$ ). The relative contributions of these two  
 189 components are given by  $\rho$ . The third component  $\sigma^2 \mathbf{W} \mathbf{W}^T$  reflects variance (with magnitude  $\sigma^2$ )  
 190 shared between voxels with similar orientation preference (given by  $\mathbf{W} \mathbf{W}^T$ ).

191 The voxel tuning functions and covariance matrix together model the generative distribution of  
 192 activation patterns:

$$193 \quad p(\mathbf{b}|s, \theta) = N(\mathbf{W}\mathbf{f}(s), \mathbf{\Omega})$$

194 which is a multivariate normal distribution with mean  $\mathbf{W}\mathbf{f}(s)$  and covariance  $\mathbf{\Omega}$ .  $\theta = \{\mathbf{W}, \rho, \boldsymbol{\tau}, \sigma\}$  are  
195 the generative model's parameters.

196 For model training and testing, a leave-one-run-out cross-validation procedure was used to prevent  
197 double-dipping. The model's parameters were estimated on a dataset consisting of data from all but  
198 one task run. The trained model was then tested on the held-out run, and this procedure was repeated  
199 until all runs had served as a test run exactly once. The parameters were estimated in two steps: the  
200 coefficients  $\mathbf{W}$  were first estimated by ordinary least squares regression, and then the covariance  
201 parameters  $(\rho, \boldsymbol{\tau}, \sigma)$  were estimated through numerical likelihood maximization (see van Bergen et al.,  
202 2015 for further details regarding model estimation procedures).

203 Model testing ('decoding') consisted of calculating a posterior distribution  $p(s|\mathbf{b}, \hat{\theta})$  over stimulus  
204 orientation  $s$ , conditioned on the response pattern  $\mathbf{b}$  and estimated parameters  $\hat{\theta}$ . The posterior  
205 distribution is given by Bayes' rule:

$$206 \quad p(s|\mathbf{b}, \hat{\theta}) = \frac{p(\mathbf{b}|s, \hat{\theta})p(s)}{\int p(\mathbf{b}|s, \hat{\theta})p(s)}$$

207 The stimulus prior  $p(s)$  was flat, reflecting the uniform stimulus distribution used in the experiment.  
208 The normalization constant  $\int p(\mathbf{b}|s, \hat{\theta})p(s)$  was computed numerically. The circular mean of the  
209 decoded distribution was taken as the decoder's estimate of the presented orientation ('decoded  
210 orientation') and the squared circular standard deviation quantified the uncertainty in this estimate  
211 ('decoded uncertainty').

## 212 Preprocessing of pupil data

213 Blinks and saccades were identified using the Eyelink software. Data recorded during saccades or less  
214 than 250 ms before (after) blink onset (offset) were removed. Missing or removed data were linearly  
215 interpolated. Data interpolated over more than 1000 ms were removed at the end of the preprocessing

216 procedure. If more than 50 % of the data in a given trial were missing, the trial was excluded from pupil  
217 data analyses.

218 The pupil's responses to blinks and saccades were estimated and regressed out using a deconvolution  
219 approach developed by Knapen et al. (2016), and implemented by Urai et al. (2017). Specifically, the  
220 shape of blink- and saccade-triggered pupil responses was first estimated by fitting a finite impulse  
221 response (FIR) model to the data of each participant. The estimated response was then used to create  
222 a regressor in a linear regression analysis, and blink- and saccade-related effects were removed  
223 (separately for each run). Data were subsequently low-pass filtered using a third-order Butterworth  
224 filter with a cut-off of 4 Hz, and downsampled to 100 Hz. Global effects in the data (cf. Knapen et al.,  
225 2016) were removed by fitting an exponential function to each run and using the residuals of this fit in  
226 subsequent analyses. Finally, pupil size was z-normalized per session to correct for differences in  
227 camera and lighting position between sessions.

228 We considered both the pupil size time series and its first derivative as indices of arousal. To estimate  
229 the derivative, we used a moving window with a width of 500 or 1000 ms. Within this window, we  
230 fitted a linear function to the pupil time series. We took the slope of this fitted function as a measure  
231 of the rate of change in pupil size at the time point on which the moving window was centered.

## 232 **Preprocessing of behavioral data**

233 The error in the observer's orientation response on a given trial was calculated as the acute-angle  
234 difference between the presented and reported orientation. Participants generally performed well on  
235 the task, with a mean absolute orientation response error of  $5.81 \pm 1.29$  degrees (mean  $\pm$  s.d. across  
236 observers). To correct for orientation-dependent biases in the response (shifts in mean response), two  
237 fourth-degree polynomials modeling response error as a function of stimulus orientation were fit to  
238 each participant's data (van Bergen et al., 2015; Geurts et al., 2022). The first polynomial was fit to  
239 trials with presented stimulus orientation between 0 and 89 degrees and the second to trials with the

240 presented stimulus between 90 and 179 degrees. The residuals of these fits ('bias-corrected behavioral  
241 responses') were used in subsequent analyses. Trials on which the bias-corrected response was more  
242 than three standard deviations away from zero were marked as guesses and excluded from all further  
243 analyses ( $0.91 \pm 0.31$  percent of all trials; mean  $\pm$  s.d. across observers). Confidence ratings were z-  
244 scored per session to correct for potential between-participant or between-session differences in  
245 usage of the confidence scale. We excluded trials on which observers did not finish adjusting their  
246 orientation and/or confidence response before the end of the response window ( $2.75 \pm 2.40$  percent  
247 of all trials; mean  $\pm$  s.d. across observers).

## 248 **Statistical procedures**

249 To benchmark our decoding approach, we quantified orientation decoding performance by calculating  
250 the circular equivalent of Pearson's correlation coefficient between the presented and decoded  
251 orientation across trials and for each individual observer. To quantify the effect at the group level, the  
252 single-observer correlation coefficients were Fisher-transformed, and a weighted average was  
253 computed. The weight for the correlation coefficient of observer  $i$  was calculated as  $w_i = \frac{1}{v_i}$ , where  $v_i$   
254 corresponds to the variance of the Fisher-transformed correlation coefficient (Hedges and Olkin,  
255 1985). This variance is given by  $v_i = \frac{1}{n_i - 3}$ , in which  $n_i$  represents the number of trials. Statistical  
256 significance of the group-averaged correlation coefficients was assessed using a Z-test. The results  
257 from this analysis, as well as the correlation between decoded uncertainty and distance to the nearest  
258 cardinal axis and behavioral variability (see below), were also reported as benchmarks in a previous  
259 study (Geurts et al., 2022, Extended Data Figure 2).

260 To assess whether decoded uncertainty predicts behavioral variability, trials were divided into ten bins  
261 of increasing uncertainty for each individual observer. Mean decoded uncertainty was computed  
262 across all trials in each bin and behavioral variability was quantified as the squared circular standard  
263 deviation of the (bias-corrected) behavioral errors in the bin. Multiple linear regression was performed

264 to calculate the partial correlation coefficient for the relationship between decoded uncertainty and  
265 behavioral variability at the group level, with separate intercepts for each observer. Statistical  
266 significance was assessed by means of a t-test. We performed a number of control analyses, in which  
267 we varied several analysis parameters. First, because there is no principled way for determining the  
268 number of bins to use in this analysis, we ran two additional analyses using five or fifteen (instead of  
269 ten) uncertainty bins per participant. Second, because the strength of the link between decoded  
270 uncertainty and behavioral variability could vary across individuals, we performed a linear mixed-  
271 effects analysis (using MATLAB's *lmeffit* function) in which both the intercept and the slope were  
272 modeled as random effects. This is in contrast to the multiple linear regression approach described  
273 above, which assumes that the intercepts are random variables while the slope is fixed. Third, to assess  
274 the influence of extreme values, we performed the analysis on different subsets of the data. The first  
275 subset excluded all trials for which the standard deviation of the decoded distribution was larger than  
276 45 degrees. In the second subset, we simply excluded from our analyses the observer who gave rise to  
277 the data point in the top-right corner of Figure 2B. Statistical significance was assessed by means of t-  
278 tests on the partial correlation coefficients ( $r$ ) or estimated slope ( $\beta$ ) for the multiple regression and  
279 linear mixed effects analyses, respectively. In the linear mixed effects analysis, Satterthwaite  
280 approximation was used to estimate the effective degrees of freedom.

281 The relationship between pupil size and decoded uncertainty or reported confidence was tested in two  
282 different ways. For the first set of analyses, we divided trials into three bins per observer, based on the  
283 level of decoded uncertainty (or reported confidence), and compared pupil size between the highest  
284 and lowest bin. We computed t-values to quantify the difference between these bins. T-values were  
285 computed for each observer individually, and then averaged across observers. The analysis was  
286 performed for each time point within the window of interest; that is, from 1.5 s before stimulus onset  
287 until 1.5 s after stimulus offset. To assess statistical significance, threshold-free cluster enhancement  
288 (TFCE; Smith and Nichols, 2009) and permutation testing (1000 permutations) were used. The family-

289 wise error rate (FWER) was controlled by comparing the true single-timepoint TFCE scores against the  
290 null distribution of the maximum TFCE score across time obtained through data permutation (Nichols  
291 and Hayasaka, 2003).

292 In the second set of analyses, we quantified the relationship between pupil size (or slope) and decoded  
293 uncertainty (or reported confidence) on a trial-by-trial basis. To do so, we computed Spearman's  
294 correlation coefficient for each data point in the pupil time series, from 1.5 s before stimulus onset  
295 until 1.5 s after stimulus offset. Spearman's correlation coefficient was used because there is no a-  
296 priori reason to assume that the relationship should be linear. Correlation coefficients were computed  
297 for each observer individually and group-level correlation coefficients were calculated following similar  
298 procedures as for orientation decoding performance. Specifically, individual correlation coefficients  
299 were Fisher transformed and a weighted average was computed with weights  $w_i = \frac{1}{v_i}$  (Hedges and  
300 Olkin, 1985). For Spearman's correlation coefficient,  $v_i$  is given by  $v_i = \frac{1.06}{n_i - 3}$ , with  $n_i$  representing the  
301 number of trials for observer  $i$  (Fieller and Pearson, 1961). As before, statistical significance was  
302 assessed using TFCE and permutation testing (1000 permutations), and the FWER was controlled by  
303 comparing against the null distribution of the maximum TFCE-value across time points.

304 For the visualizations in Figure 4D, pupil size was averaged over the stimulus presentation window on  
305 a trial-by-trial basis. Spearman correlation coefficients between decoded uncertainty and (mean) pupil  
306 size were computed per observer, Fisher-transformed and averaged as described above. Z-tests were  
307 used to assess significance both at the group level and for the example observer.

308 The relative effect size of arousal state on changes in uncertainty was determined as follows. Because  
309 the effect size cannot be determined directly from the observed relationship between arousal and  
310 uncertainty (decoded uncertainty reflects not only neural but also many non-neural sources of noise,  
311 including from the fMRI scanner), we instead relied on an indirect approach and compared the effect  
312 of pupil-linked arousal with that of a manipulation of stimulus orientation to acquire an understanding

313 of its relative contribution. The impact of stimulus orientation on decoded uncertainty was quantified  
314 by computing the Spearman correlation coefficient between decoded uncertainty and the distance  
315 between the presented stimulus orientation and the nearest cardinal axis (cf. Geurts et al. 2022,  
316 Extended Data Figure 2B). Correlation coefficients were computed per observer, Fisher transformed  
317 and then averaged across observers as described above. The impact of pupil-linked arousal was  
318 summarized by first averaging pupil size over the stimulus presentation window on a per trial basis (cf.  
319 Figure 4D), and then computing and averaging the Spearman correlation coefficients between these  
320 trial-by-trial values and decoded uncertainty as described in the previous paragraph. Effect sizes were  
321 defined as the absolute group-averaged Spearman correlation coefficient.

## 322 **Code accessibility**

323 All custom analysis code is available from the corresponding author upon request. Code for the  
324 probabilistic decoding algorithm can be found at <https://github.com/jeheelab/>.



## 325 RESULTS

326 Do spontaneous fluctuations in arousal modulate the cortical representation of the stimulus? To  
327 address this question, we presented thirty-two human observers with oriented gratings while  
328 simultaneously measuring pupil size and recording their brain activity with fMRI. Observers reported  
329 the orientation of the grating and rated their level of confidence in this orientation judgment (Figure 1).  
330 To quantify the degree of imprecision in the stimulus representation in visual cortex (areas V1, V2, and  
331 V3 combined), we used a probabilistic decoding technique (van Bergen et al., 2015; van Bergen and  
332 Jehee, 2018). This technique computes a probability distribution over stimulus orientation for each  
333 trial of cortical activity (Figure 2A, top panel). The width of the decoded distribution reflects the degree  
334 of uncertainty contained in the pattern of activity. We refer to this metric as ‘decoded uncertainty’. To  
335 measure arousal, we relied on pupil recordings (Figure 2A, middle panel). That is, pupil size is an  
336 established indicator of arousal state (e.g. Aston-Jones and Cohen, 2005; Gilzenrat et al., 2010; Reimer  
337 et al., 2014; Vinck et al., 2015; de Gee et al., 2017, 2020; Urai et al., 2017; Pfeffer et al., 2022). Both  
338 physiological and neuroimaging studies have linked changes in pupil dilation to activity in the locus  
339 coeruleus (LC) and the release of noradrenaline (NE) (Aston-Jones and Cohen, 2005; Murphy et al.,  
340 2014; Varazzani et al., 2015; Joshi et al., 2016). Previous work suggests that while overall pupil size is  
341 influenced by multiple factors, rapid (phasic) changes in pupil size more specifically track activity in the  
342 LC-NE system (Reimer et al., 2016). To quantify arousal, we therefore considered both pupil size and  
343 the first derivative (‘slope’) of its timeseries, which is specifically sensitive to changes in pupil size. Note  
344 that there is an inherent link between (changes in) pupil slope and pupil size: a large (positive) pupil  
345 slope at any given moment in time should be linked to an increase in pupil size moments later. For this  
346 reason, a true change in arousal state should be reflected in the pupil signal via an effect on slope  
347 followed by one on size (albeit that the two measures need not be equally sensitive; Reimer et al.,  
348 2016).

## 349 Decoded distributions reflect presented stimulus and behavioral imprecision

350 To benchmark our decoding approach, we first tested how closely the decoder's orientation estimate  
351 (the mean of the decoded distribution) matched the presented orientation on a trial-by-trial basis. We  
352 computed the circular correlation coefficient between the decoded and presented orientations for  
353 each participant individually and then averaged the coefficients. This analysis revealed that the  
354 decoded and presented orientations were significantly correlated ( $z = 83.58$ ,  $p < 0.001$ ,  $r = 0.60$ ,  
355 95% CI = [0.58, 0.61], see also Extended Data Figure 2A in Geurts et al., 2022).

356 Having established that the presented orientation can reliably be extracted from cortical activity, we  
357 next asked whether the width of the decoded distribution is a meaningful measure of the degree of  
358 imprecision in the cortical stimulus representation. That is, a more precise representation in cortex  
359 should result in more precise (less variable) behavior. Is decoded width linked to behavioral variability,  
360 suggesting that it reflects the quality of the underlying neural representation? To address this question,  
361 we divided trials into bins of increasing distribution width (ten bins per participant), calculated the  
362 variance of the behavioral orientation estimates in each bin (Figure 2A, bottom panel), and quantified  
363 their relationship via a regression analysis. Replicating previous studies (van Bergen et al., 2015;  
364 Chetverikov and Jehee, 2023), this revealed a significant link between the width of the posterior  
365 distribution and behavioral variability (Figure 2B;  $t(287) = 2.30$ ,  $p = 0.011$ ,  $r = 0.13$ , 95% CI = [0.019,  
366 0.25]). Specifically, the broader the distribution's width, the more variable the observers' behavioral  
367 orientation estimates were. Control analyses, in which we varied the number of uncertainty bins, used  
368 two different statistical models (mixed versus fixed effects), and analyzed various subsets of the data  
369 (see Methods for details), showed that these results are fairly robust to changes in analysis parameters  
370 (see Figure 3 for data and statistics). Taken together, this suggests that posterior width provides a  
371 reliable measure of the degree of uncertainty contained in neural activity. Interestingly, it also shows  
372 that the imprecision in the cortical representation is not constant over trials, but rather varies from  
373 one trial to the next, with clear consequences for behavior.

## 374 Pupil-linked arousal reliably predicts decoded uncertainty

375 Our analyses revealed that uncertainty fluctuates considerably from one trial to the next. What  
376 processes might underlie these spontaneous changes in neural activity? Here, we hypothesize that  
377 fluctuations in sensory uncertainty might be linked to arousal state. That is, given that arousal is a  
378 physiological state of alertness with effects on neural activity (Livingstone and Hubel, 1981; Reimer et  
379 al., 2014; Vinck et al., 2015), we reasoned that higher levels of arousal might lead to better stimulus  
380 representations in cortex, and hence, lower stimulus uncertainty. To measure arousal, we recorded  
381 pupil size while participants performed the task in the scanner. We predicted that the size of the pupil  
382 should vary across trials and be linked to uncertainty. Specifically, sensory uncertainty should decrease  
383 when the pupil dilates, indicating higher levels of arousal. To index arousal state, we considered both  
384 pupil size and the slope of the pupil timeseries, which quantifies the rate of change in pupil size.  
385 Because we were interested in the effects of arousal on sensory uncertainty, we focused on pupil size  
386 and dilation just before, during and just after stimulus presentation (Figure 4A). Note that while a  
387 change in pupil size alone can affect retinal resolution (which might, in turn, affect downstream  
388 activity), the direction of this effect runs opposite to what we predict here, as retinal image quality is  
389 reduced for larger pupils due to spherical aberrations (Campbell and Gregory, 1960; Campbell and  
390 Green, 1965).

391 To test the link between pupil-linked arousal and representational fidelity, we first divided all trials of  
392 each individual participant into three equal-sized bins of increasing uncertainty, computed for each  
393 point in time the mean pupil size across all trials in each bin, and then compared between the lowest  
394 and highest uncertainty bin. Paired t-tests revealed a significant difference in pupil size between high  
395 and low uncertainty trials starting just before cue onset and lasting until at least 1.5 s after stimulus  
396 offset (Figure 4B, left panel; permutation tests, all  $p < 0.05$ , FWER-corrected). Thus, the size of the pupil  
397 was larger when uncertainty in cortex was low and the stimulus representation was more precise.

398 Interestingly, the effect started well before stimulus onset, suggesting that altered arousal state led to  
399 the change in the cortical representation of the stimulus.

400 We next asked if decoded uncertainty is also linked to pupil size on a per trial basis. To address this  
401 question, we computed the trial-by-trial correlation coefficient between decoded uncertainty and  
402 pupil size (calculated separately for each time point). We did this first for each individual observer and  
403 then averaged across observers (see Methods for details). We observed a significant inverse link  
404 between decoded uncertainty and pupil size (permutation tests,  $p < 0.05$ , FWER-corrected). Thus, pupil  
405 size was reliably larger when the cortical representation of the stimulus was more precise (Figure 4C,  
406 left panel). Interestingly, the timing of the effect overlapped strongly with stimulus presentation,  
407 consistent with the idea that arousal modulates the quality of the stimulus representation in cortex.

408 We then turned to the rate at which pupil size changed prior to and during stimulus presentation. We  
409 first estimated the slope of the pupil response in a specified time window (sliding window of length  
410 500 ms and 1000 ms), and took this slope as a measure of change (see Methods). We then computed  
411 the across-trial correlation coefficient between pupil slope and decoded uncertainty. This revealed a  
412 significant inverse relationship between pupil slope and decoded uncertainty prior to the onset of the  
413 cue (permutation tests,  $p < 0.05$ , FWER-corrected; see Figure 4C, left panel and inset, 500 and 1000 ms  
414 windows), which lasted until the onset of the stimulus (Figure 4C, left, inset, 1000 ms window; see  
415 Figure 4D for individual correlation coefficients and an example observer). Thus, it appears that pupil  
416 size first dilates in anticipation of the stimulus, and then remains constant at increased size during  
417 stimulus presentation (Figure 4C left panel and inset). Taken together, our analyses show that there is  
418 a reliable relationship between decoded uncertainty and both pupil size and dilation. This altogether  
419 suggests that spontaneous fluctuations in arousal state result in an improved representation of  
420 stimulus orientation in the human visual cortex.

## 421 Relationship between pupil-linked arousal and reported confidence

422 The participants not only reported the presented orientation, but also gave their level of confidence  
423 in this judgment. We previously showed, using the same dataset as here, that reported levels of  
424 confidence are linked to both behavioral performance and the precision of the cortical stimulus  
425 representation. This suggests that subjective confidence is computed from the degree of uncertainty  
426 in cortex (Geurts et al., 2022). Based on this relationship, we here asked whether pupil-linked arousal  
427 also predicts confidence. In other words, we took reported confidence as an (indirect) measure of the  
428 degree of uncertainty in cortex to see if it is linked to the pupil's response. To address this question,  
429 we again divided the data for each individual observer into three bins of increasing confidence,  
430 computed the mean pupil size across all trials in each bin (separately for each time point), and  
431 combined the data across observers (see Methods). We compared pupil size between the first (lowest)  
432 and third (highest) confidence bins (Figure 4B, right panel). This analysis revealed a significant  
433 difference in pupil size between the high and low confidence bins, starting around 0.5-0.6 s after  
434 stimulus onset and lasting until about 1.5 s after stimulus offset (t-tests; all  $p < 0.05$ , FWER-corrected).  
435 That is, higher levels of confidence were reliably associated with greater pupil size, suggesting that  
436 arousal state affects the subjective level of confidence of the observers.

437 We next analyzed the data on a trial-by-trial basis. Specifically, much like before, we computed for  
438 each individual observer the correlation coefficient between reported confidence and pupil size (for  
439 each time point) or slope (computed over a specified sliding window of time), and combined the data  
440 across observers (Figure 4C, right panel). While we observed no reliable link with pupil size, there was  
441 a significant positive relationship between reported confidence and pupil slope during stimulus  
442 presentation (0.3-0.9 s after stimulus onset;  $p < 0.05$ , FWER-corrected). Thus, the steeper was the slope  
443 of the pupil's response, the more confident the observers were about their orientation judgments.  
444 Because stronger pupil dilation (or weaker constriction) is associated with higher levels of arousal

445 (Reimer et al., 2016), this altogether suggests that arousal state modulates both the cortical  
446 representation of orientation and reported confidence.

#### 447 **Pupil-linked arousal is linked to behavior**

448 Is the link between arousal state and the quality of the cortical stimulus representation also reflected  
449 in behavior? We reasoned that if arousal state modulates the precision of information in cortex, it  
450 should similarly impact behavior. We tested this hypothesis as follows. We first divided, per participant  
451 and time point, all trials into ten bins of increasing pupil size or slope. We then quantified behavioral  
452 imprecision as the variance in the orientation estimation errors in each bin, and performed a multiple  
453 linear regression analysis to compute the partial correlation coefficient between pupil size or slope and  
454 behavioral variability, while controlling for interindividual differences in the mean. Our results indicate  
455 that pupil-linked arousal boosts behavioral performance, much like it improves neural precision.  
456 Specifically, we observed a reliable inverse correlation between pupil slope and behavioral variability  
457 prior to and during stimulus presentation (permutation tests,  $p < 0.05$ , FWER-corrected). The  
458 correlation coefficient between pupil size and behavioral variability during and immediately after  
459 stimulus presentation was also negative and significant (permutation tests,  $p < 0.05$ , FWER-corrected;  
460 Figure 5). In other words, orientation estimates were more precise on trials with stronger pupil dilation  
461 just before and during stimulus presentation, indicating a state of higher arousal. This shows that  
462 spontaneous fluctuations in arousal state manifest themselves not only at the neural level, but also in  
463 behavior.

#### 464 **Assessing the relative magnitude of the effect of arousal on uncertainty**

465 Our findings suggest that arousal state modulates the precision of the cortical stimulus representation.  
466 However, it remains unclear how large the impact is of arousal on representational precision in cortex.  
467 The size of arousal's impact cannot be taken directly from its relationship with decoded uncertainty  
468 (i.e., from the magnitude of the obtained correlation coefficient), as decoded uncertainty reflects not

469 only neural but also many non-neural sources of noise, including from the MRI scanner. Similarly, pupil  
470 size is not a direct read-out of arousal state, and likely also reflects many other physiological processes.  
471 For this reason, we instead relied on an indirect approach and compared arousal's effect on  
472 uncertainty with that of stimulus orientation to acquire an understanding of their relative contribution  
473 in cortex. Behavioral accuracy and cortical activity are well known to vary across orientation stimuli,  
474 with poorer behavioral performance and reduced representational fidelity for oblique compared to  
475 cardinal orientations (Appelle, 1972; Furmanski and Engel, 2000; van Bergen et al., 2015). We also  
476 observed this oblique effect in our own data, with greater decoded uncertainty and larger behavioral  
477 variability for oblique compared to cardinal orientation stimuli (correlation between distance-to-  
478 cardinal and decoded uncertainty or behavioral variability, respectively:  $\rho = 0.025$ ,  $z = 2.95$ ,  $p = 0.002$ ,  
479 and  $r = 0.63$ ,  $t(287) = 13.60$ ,  $p < 0.001$ ; Figure 6A; see also Geurts et al., 2022, Extended Data Figure  
480 2B). To assess the relative impact of pupil-linked arousal on representational imprecision, we  
481 compared the absolute effect sizes ( $|\rho|$ ) between the two. Interestingly, we found that the impact of  
482 pupil-linked arousal on decoded uncertainty is of the same order of magnitude as that of stimulus  
483 orientation ( $|\rho| = 0.025$  versus  $|\rho| = 0.023$  for orientation and arousal, respectively, Figure 6B). This  
484 suggests that arousal state has a rather significant influence on representational fidelity in cortex –  
485 almost as large as that of a physical change in stimulus orientation.

## 486 DISCUSSION

487 Do spontaneous fluctuations in arousal state affect the quality of stimulus information contained in  
488 visual cortical activity? Here, we addressed this question by measuring the degree of uncertainty in  
489 the cortical stimulus representation using a probabilistic decoding technique, while taking pupil size as  
490 an index of arousal state. We observed that both pupil-linked arousal and decoded sensory uncertainty  
491 fluctuate over trials. Moreover, we discovered that these trial-by-trial fluctuations in arousal state are  
492 linked to the uncertainty contained in visual cortical activity. Specifically, trials of low sensory  
493 uncertainty differed from high uncertainty trials in that the pupil rapidly dilated just prior to stimulus  
494 onset, followed by sustained levels of increased pupil size during stimulus presentation, when  
495 uncertainty was low. Because rapid pupil dilation is a hallmark of a change in arousal state, this  
496 suggests that arousal affects the degree of uncertainty in the cortical representation of the stimulus.  
497 Interestingly, we observed a similar relationship between pupil size and subjective confidence, a  
498 secondary measure of sensory uncertainty, and between the pupil's signals and behavioral  
499 performance. A comparison between the effects of pupil-linked arousal and those of stimulus  
500 orientation suggested that arousal's impact on representational imprecision was almost as large as  
501 that of a physical change in the stimulus. Taken together, these results suggest that arousal state has  
502 reasonably large impact on the fidelity of information processing in the human visual cortex, with clear  
503 consequences for behavior.

504 A key distinguishing aspect of this study is that we measured the precision of the neural representation  
505 directly in cortex, using a probabilistic decoding technique that enabled us to quantify representational  
506 imprecision as the width of a probability distribution over possible stimuli. Previous studies using this  
507 technique have shown that this imprecision in the cortical stimulus representation varies from trial to  
508 trial, even when the stimulus is held constant (van Bergen et al., 2015; Geurts et al., 2022; Chetverikov  
509 and Jehee, 2023). Consistent with Bayesian theories of decision-making, these changes in imprecision  
510 have moreover been shown to affect the observer's decision-making, with larger uncertainty resulting



511 in enhanced perceptual biases (van Bergen et al., 2015; van Bergen and Jehee, 2019), lower reported  
512 confidence (Geurts et al., 2022), and different perceptual choices (Walker et al., 2020). It remained  
513 unclear, however, what drives such stimulus-independent fluctuations in sensory cortical uncertainty.  
514 The present work builds on and extends this line of research, suggesting that arousal is one of the  
515 factors influencing the imprecision in neural representations.

516 Contrary to previous studies investigating the effect of arousal on neural activity in humans (e.g. Keil  
517 et al., 2003; Warren et al., 2016; Gelbard-Sagiv et al., 2018), we did not explicitly manipulate arousal,  
518 but specifically focused on spontaneous fluctuations. That is, we were interested in what drives  
519 variability in the precision of neural representations in the absence of external, experimentally  
520 manipulated change. We used pupil size as an index of arousal, because of its well-established links to  
521 the neuromodulatory systems underlying arousal (Aston-Jones and Cohen, 2005; Murphy et al., 2014;  
522 Varazzani et al., 2015; Joshi et al., 2016). Interestingly, our findings are consistent with earlier work in  
523 which catecholamine (noradrenaline and dopamine) levels were manipulated pharmacologically and  
524 representational precision was measured across trials (Warren et al., 2016). Here we show that the  
525 relationship between arousal and representational precision similarly holds on a trial-by-trial basis and  
526 in the absence of explicit manipulations of arousal or noradrenaline levels.

527 What are the neural mechanisms by which arousal could modulate the precision of the stimulus  
528 representation in the human visual cortex? Behavioral studies in humans have reported greater  
529 contrast sensitivity with an increase in arousal (Lee et al., 2014; Kim et al., 2017), possibly mediated by  
530 multiplicative effects on the underlying cortical response (Kim et al., 2017). Neurophysiological studies  
531 in mice and rabbits have shown that an increase in arousal results in enhanced, more selective and  
532 reliable responses to visual stimuli, and weaker noise correlations (Cano et al., 2006; Niell and Stryker,  
533 2010; Erisken et al., 2014; Reimer et al., 2014; Vinck et al., 2015) – mechanisms that could all lead to  
534 an increase in the amount of information contained in neural activity. Theoretical work has linked  
535 arousal to changes in neural response gain (Servan-Schreiber et al., 1990; Aston-Jones and Cohen,

536 2005), which could similarly improve the quality of the information encoded in neural activity and, as  
537 such, reduce sensory uncertainty (Seung and Sompolinsky, 1993; Ma et al., 2006). Indeed, one  
538 neurophysiological study in monkeys directly related spontaneous fluctuations in activity (as we relied  
539 on here) to changes in neural excitability or gain (Goris et al., 2014). It altogether seems plausible that  
540 one of these mechanisms, or a combination thereof, could mediate arousal-linked fluctuations in  
541 sensory uncertainty in the human visual cortex.

542 It is important to realize that we do not intend to argue that arousal is the sole driver of spontaneous  
543 fluctuations in cortical information. For example, it is well known that attending to a visual feature or  
544 location improves its representation in cortex (Kamitani and Tong, 2005; Saproo and Serences, 2010;  
545 Jehee et al., 2011). Attention has also been shown to modulate pupil size (see Strauch et al., 2022 for  
546 a review). It is highly conceivable that also attention-based processes spontaneously wax and wane  
547 and affect the amount of information in cortex, much like we observed for arousal here. One way to  
548 distinguish between these processes could be to focus on the different neural systems that mediate  
549 their effects, such as the LC for arousal (Moruzzi and Magoun, 1949; Berridge and Waterhouse, 2003;  
550 Aston-Jones and Cohen, 2005; Sara and Bouret, 2012). However, the current study was not designed  
551 nor optimized for this research question. Nevertheless, a preliminary analysis showed hints of a link  
552 between LC activity and decoded uncertainty in our dataset, which further supports the notion that  
553 changes in arousal state underlie the observed uncertainty fluctuations. It will be interesting for future  
554 studies to further investigate and disentangle these and other cognitive processes that give rise to  
555 spontaneous fluctuations in neural information.

556 Taken together, we showed that spontaneous, trial-by-trial fluctuations in arousal state, as indexed by  
557 pupil size, are linked to the quality of visual cortical stimulus representations, as well as reported levels  
558 of subjective confidence and behavioral performance. This suggests that arousal is one of the driving

559 factors of variability in neural responses and the precision with which sensory information is encoded  
560 in cortical activity.

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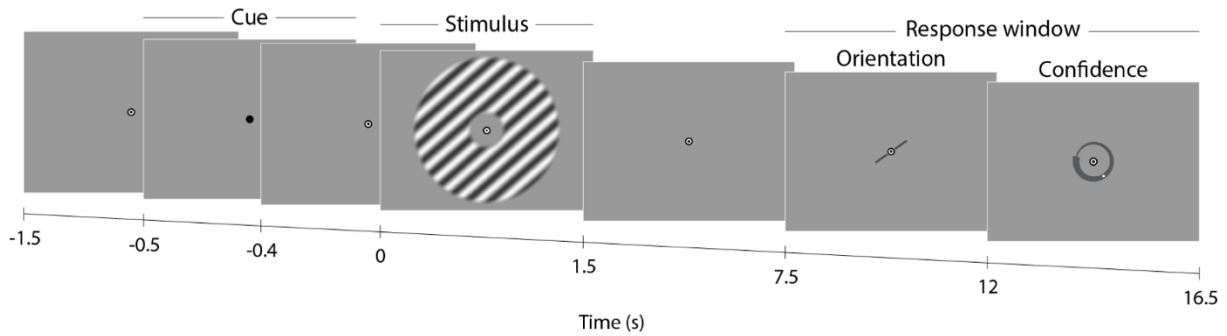
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692

693 FIGURE LEGENDS

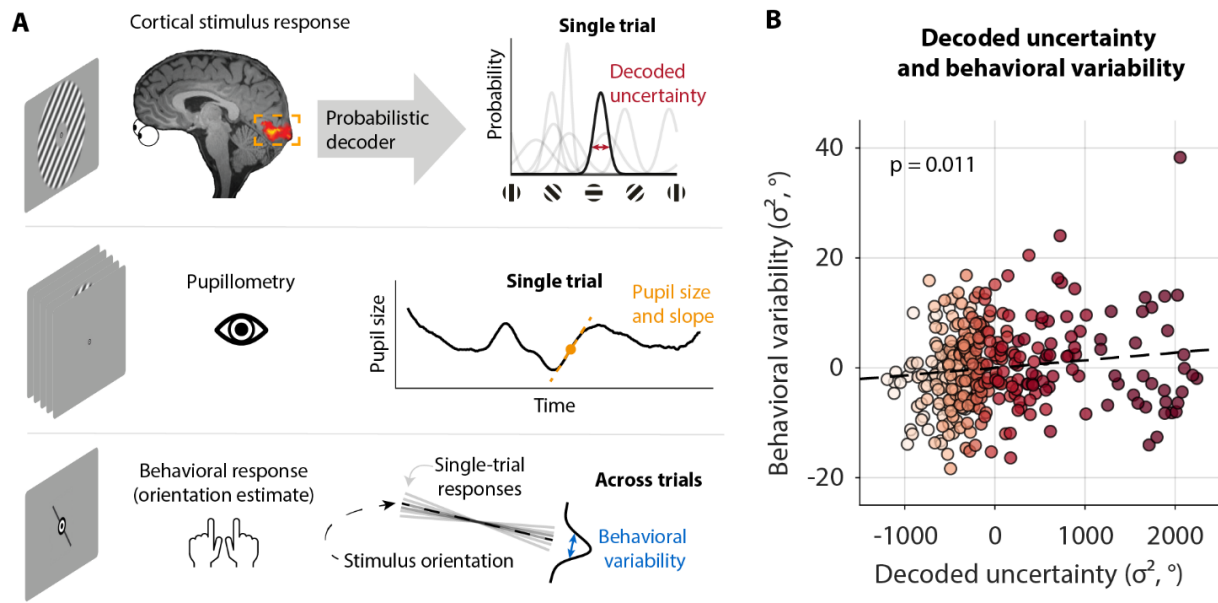


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695 **Figure 1: Overview of the orientation estimation task.** Participants were required to fixate the  
696 bullseye target in the center of the screen throughout each run. Each trial started with this bullseye  
697 briefly turning black, as a cue to stimulus onset. The visual stimulus was a counterphasing sinusoidal  
698 grating, presented in an annulus around fixation, and was presented for 1.5 s. After a 6 s-delay (fixation  
699 interval), a black bar appeared in the center of the screen, and participants were required to report  
700 their orientation estimate by rotating this bar. Next, they reported their level of confidence about this  
701 estimate by sliding a dot over the (circular) confidence scale. Both response intervals lasted for 4.5 s,  
702 and the bar or scale started fading after 3.5 s to indicating the approaching end of the response  
703 window. A 1.5-s intertrial interval separated the response window from the next stimulus. Participants  
704 completed 20 trials per run.

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708 **Figure 2: Overview of behavioral, physiological, and neural measures and behavioral benchmarking.**

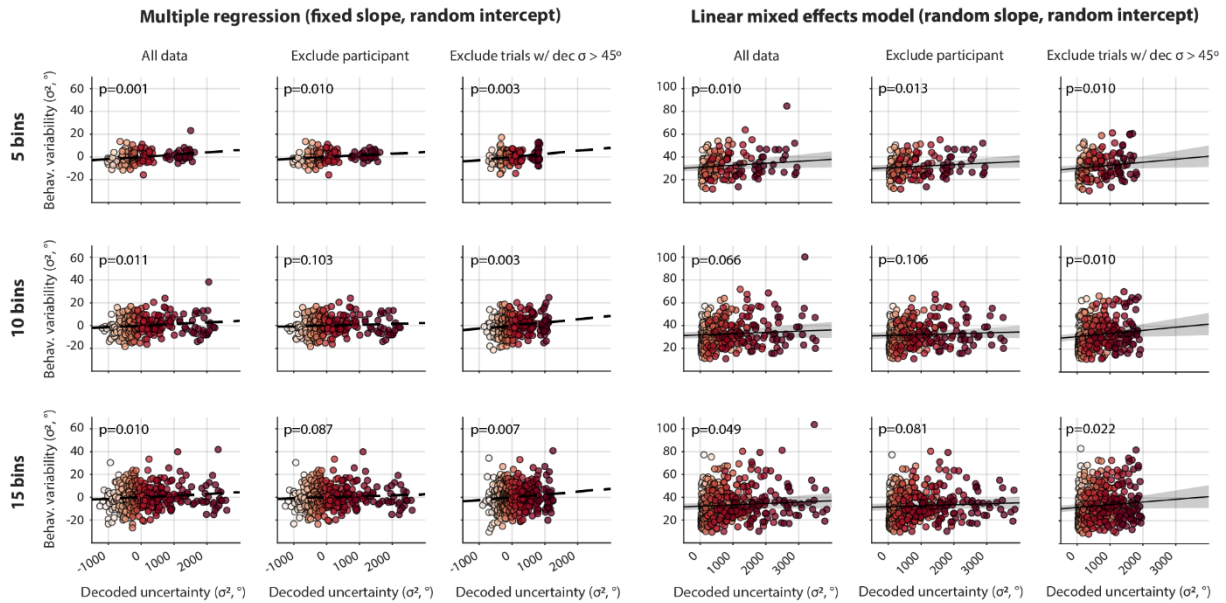
709 A) The imprecision in the cortical stimulus representation was quantified using a probabilistic decoding  
 710 technique. This decoding algorithm computes a probability distribution over stimulus orientation from  
 711 single-trial activity patterns. The width of the distribution was taken as a measure of the degree of  
 712 uncertainty in the cortical stimulus representation. The observer's perceptual uncertainty was  
 713 quantified by the width of the distribution of behavioral responses across trials. Pupil size and the slope  
 714 (the first temporal derivative) of the pupil signal were used to measure arousal over the course of each  
 715 trial. Behavioral imprecision was measured as the variability in the observer's orientation judgments  
 716 across trials. B) Decoded uncertainty predicts behavioral variability on a trial-by-trial basis. Each  
 717 observer's trials were split into ten bins of increasing decoded uncertainty. Behavioral variability was  
 718 computed as the squared circular standard deviation of behavioral response errors in each bin. The  
 719 partial correlation coefficient between decoded uncertainty and behavioral variability (controlling for  
 720 difference in intercept between participants) was computed and found to be significantly positive  
 721 ( $t(287) = 2.30$ ,  $p = 0.011$ ,  $r = 0.13$ ,  $95\% \text{ CI} = [0.019, 0.25]$ ). Thus, when the cortical stimulus  
 722 representation was more uncertain, behavioral imprecision was larger, as well. Note that the data is  
 723 centered around zero because this is a partial correlation plot so interindividual differences in the



724 mean have been removed. The fMRI results in (B) were also reported in Geurts et al. (2022), Extended  
725 Data Fig. 2.

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**Figure 3: Control analyses for the relationship between decoded uncertainty and behavioral**

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**variability.** Three parameters were varied in the analyses: 1) The number of uncertainty bins; that is,

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five, ten or fifteen bins per participant. 2) The statistical model; specifically, we modeled the strength

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(slope) of the effect as a fixed effect (multiple regression) or as a random effect (linear mixed-effects

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model). 3) The exclusion criteria; specifically, we either excluded the observer who gave rise to the

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extreme data point in the top-right corner, or excluded all trials on which the decoded level of

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uncertainty was unrealistically high (S.D. of the decoded distribution > 45 degrees). The reasoning

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behind the latter approach is that such very high values of decoded uncertainty (corresponding to a

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very wide or almost flat decoded distribution) likely reflect non-neural sources of noise related to, for

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example, the MRI scanner. We found that our results are fairly robust to these changes in analysis

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parameters. In fact, we even observed a *stronger* relationship between decoded uncertainty and

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behavioral variability when trials with unrealistically high decoded uncertainty were removed

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altogether. This shows that the observed positive correlation coefficient between decoded uncertainty

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and behavioral variability is not driven by extreme values, and strengthens our conclusion that

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decoded uncertainty reflects the precision of the underlying neural representation. Please note that

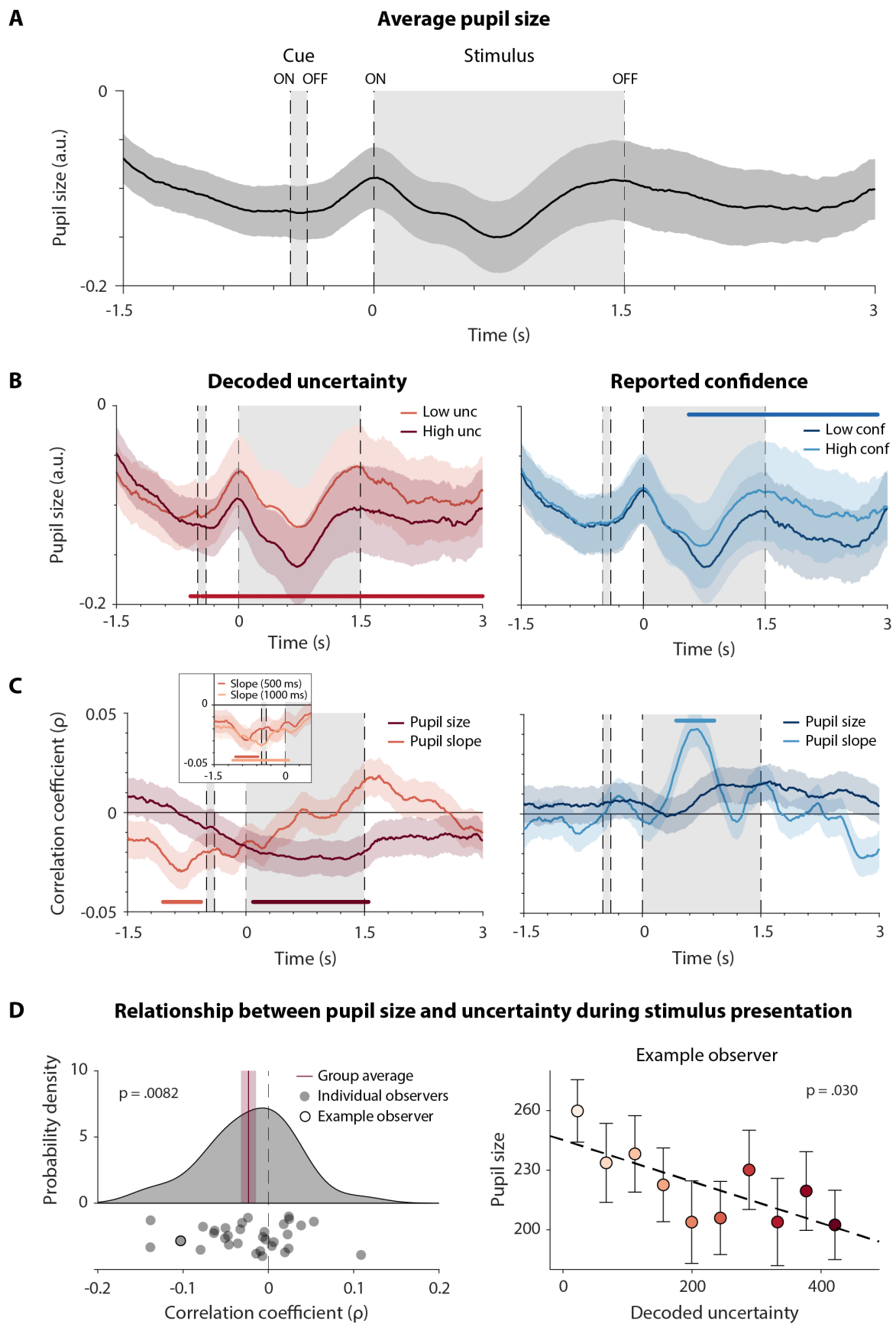
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this replicates previous findings (van Bergen et al., 2015; Chetverikov and Jehee, 2023).

745 Data points represent individual observers and colors indicate bin numbers (1-5, 1-10, or 1-15  
746 depending on the number of bins used). Dashed lines indicate the best (linear) fit, shaded area  
747 represents 95% confidence interval. For multiple regression, partial residuals are shown, which is why  
748 the data are centered around zero.

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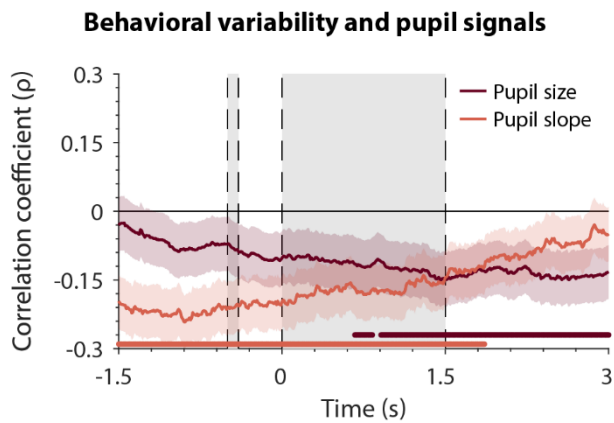
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753 **representation.** A) Mean pupil size over time. The cue appeared at -0.5 s and lasted for 0.1 s, and the  
754 stimulus was on screen from 0 to 1.5 s (0 is when the stimulus appeared on the screen). B) Pupil size  
755 timeseries separated for high and low decoded uncertainty (left) or reported confidence (right). Trials  
756 were divided into three bins of increasing uncertainty (confidence); shown are the first and third bin.  
757 C) Trial-by-trial Spearman correlation coefficients between pupil size or slope (500 ms sliding window)  
758 and decoded uncertainty (left) or reported confidence (right). Inset in left panel shows correlation  
759 between decoded uncertainty and pupil slope for two sliding windows of different length (500 and  
760 1000 ms). A-C) Shaded areas represent the standard error of the mean (s.e.m.) across observers. Bars  
761 indicate significance (permutation tests,  $p < 0.05$ , FWER-corrected). D) Relationship between decoded  
762 uncertainty and pupil size during stimulus presentation. Pupil size was averaged over the stimulus  
763 presentation window to obtain a single value per trial. Left: Distribution of Spearman correlation  
764 coefficients for individual observers, and group average (shaded area indicates s.e.m.). Right:  
765 Relationship between pupil size and decoded uncertainty for an example observer. Decoded  
766 uncertainty and pupil size were ranked, trials were subsequently divided into ten bins based on  
767 decoded uncertainty, and the data was averaged within each bin. Error bars represent s.e.m. across  
768 trials.

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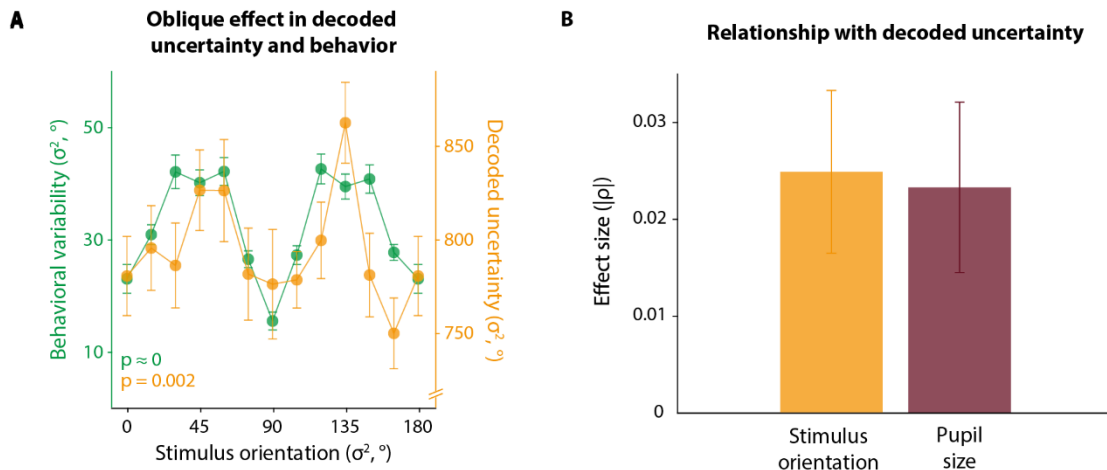


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772 **Figure 5: Behavioral imprecision is linked to arousal state.** The correlation between pupil size or slope  
 773 and behavioral variability was calculated for each point in time, in a window from 1.5 s before stimulus  
 774 onset until 1.5 s after stimulus offset. For each time point and participant, trials were divided into ten  
 775 bins of increasing pupil size (slope), and the variance in behavioral orientation judgments was  
 776 computed per bin. The correlation coefficient between pupil measures and behavioral variability was  
 777 computed while controlling for differences in mean (intercept), and is plotted over time. We observed  
 778 that increased pupil-linked arousal – as indicated by both pupil slope and size – results in more precise  
 779 (less variable) behavioral responses. Shaded areas represent the standard error of the partial  
 780 correlation coefficients. Bars indicate significance (permutation tests,  $p < 0.05$ , FWER-corrected).  
 781 Dashed lines indicate on- and offsets of the cue and stimulus.

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785 **Figure 6: Effect sizes of arousal state and stimulus orientation are comparable.** A) Decoded  
 786 uncertainty is greater for oblique compared to cardinal orientation stimuli (correlation between  
 787 distance-to-cardinal and decoded uncertainty:  $\rho = 0.025$ ,  $z = 2.95$ ,  $p = 0.002$ ). This finding is paralleled  
 788 by imprecision in the observer's behavior (correlation between distance-to-cardinal and behavioral  
 789 variability:  $r = 0.63$ ,  $t(287) = 13.60$ ,  $p < 0.001$ ). B) The strength of uncertainty's relationship with  
 790 stimulus orientation,  $|\rho| = 0.025$ , is comparable to that with pupil-linked arousal,  $|\rho| = 0.023$ . Pupil  
 791 size was averaged over the stimulus presentation window to obtain a single value per trial, and then  
 792 correlated with trial-by-trial decoded uncertainty. Panel (A) was also reported in Geurts et al. (2022),  
 793 Extended Data Fig. 2, and is reproduced here for convenience.