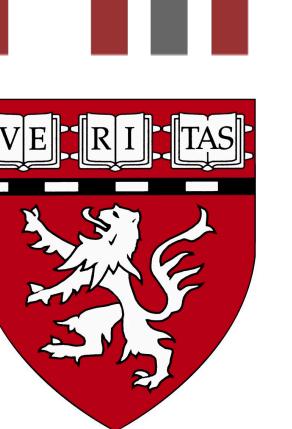
Neural Correlates of Individual Differences in Categorical Perception

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Speech is a continuous acoustic signal usually perceived categorically. Behaviorally, this looks like:

- less consistent labeling of the same sound over multiple trials (Is this a /ba/ or a /da/?);
- a shallower labeling function slope over an acoustic continuum (/ba/ to /da/ in 10 equal steps);
 weaker discrimination of sounds across a phonemic boundary (Same or different? /ba/ vs. /da/);
- stronger discrimination of sounds within a phonemic category (Same or different? /ba/1 vs. /ba/2).

Atypical, more continuous perception of speech – especially consonants – has been linked to communication/learning disorders such as dyslexia [1]. To understand the cause of this behavioral difference, we investigated the structure of phonetic and phonemic representations in the brain using univariate and multivariate analyses of MEG responses.

How does the brain respond to phonemic vs. phonetic auditory deviants?

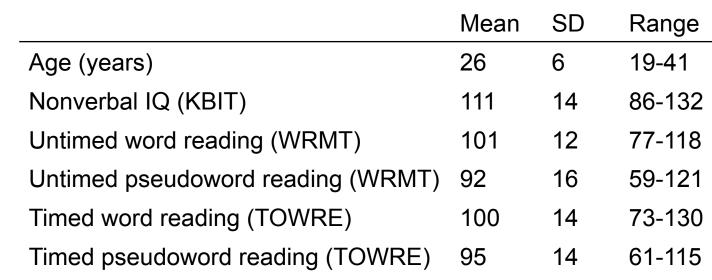
Can phonemic vs. phonetic structure be decoded from patterns of neural activity?

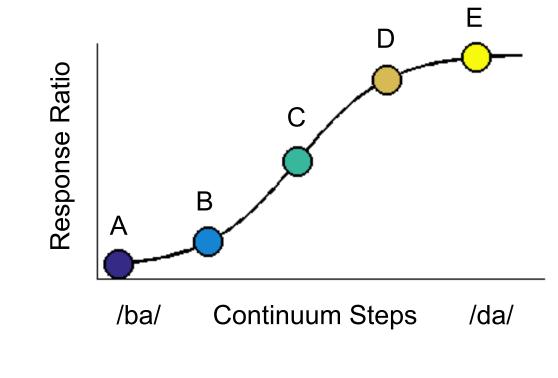
Participants were 33 adults (17 female) with normal hearing, defined as pure tone thresholds <25 dB at 0.25, 0.5, 1, 2, 4, 8 kHz. Thirteen met research criteria for dyslexia.

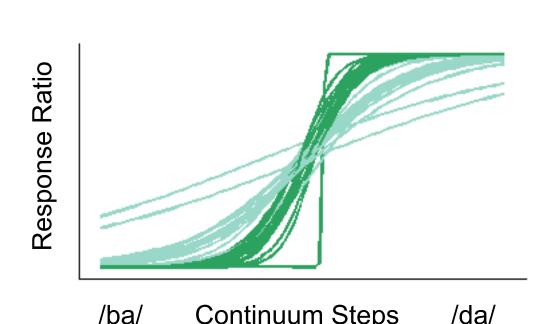
Stimulus Selection for the MEG paradigm occurred during another MEG task, in which the participant labeled tokens from a 10-step /ba/-/da/ acoustic continuum [2]. Forty trials of each step were administered in random order and the participant pressed a button to respond /ba/ or /da/. The task was self-paced with no feedback. We fit a logistic function to each individual's response ratio data. The step number nearest the inflection point was chosen as stimulus C, with A and B representing within-category /ba/ tokens and D and E within-category /da/ tokens. A, B, C, D, and E were equidistant.

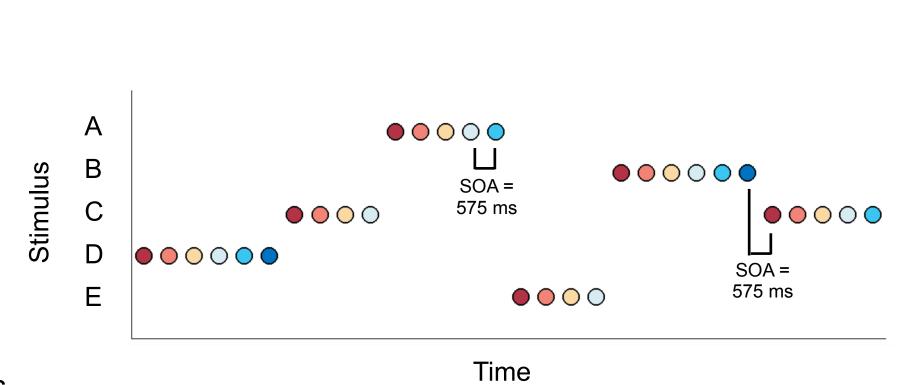
Individual Differences in slopes were evident, irrespective of dyslexia/control status. We therefore performed some analyses on the whole group, and others on a median split (n=15 steepslope participants and n=15 shallow-slope).

The **MEG Paradigm** was a roving-oddball design composed of "trains" of 4 to 6 repetitions of the same stimulus, A, B, C, D, or E. The first token of each train serves as a deviant, but, over time, becomes a standard for the next train. Transitions were balanced and pseudorandomized. Stimuli were delivered diotically via insert earphones. To maintain arousal, participants watched a soundless movie (Wall-E). A total of 3000 stimuli were presented in 28 minutes.









Recording of 306 MEG sensors was performed on an Elekta Neuromag TRIUX, with a sampling rate of 1 kHz and online filtering between 0.00003 and 0.33 kHz.

Preprocessing included using Maxfilter software to reduce noise and compensate for head movement. Brainstorm software was used to remove ocular artifacts via signal space projection, extract event-related epochs of -200 to 550 ms with respect to sound onset, and baseline-correct. **Source Estimation** was performed with minimum norm imaging and dipole modeling approaches.

Multivariate Analysis involved training a multiclass support vector machine (SVM) to distinguish stimuli A, B, C, D, and E using LIBSVM software and custom MATLAB scripts. We performed decoding on low-pass-filtered (0.03 kHz) individual trial data in MEG sensor space at every timepoint. Channel baseline means were removed and standard deviations were set to 1. We implemented four-fold cross-validation with 100 permutations. Classification results were averaged over participants.

